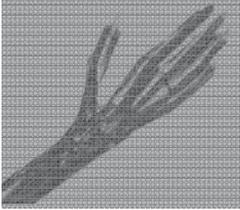


# Vibration Analysis of Finger Using Non-linear FEM to Understand HAV Syndrome

Shrikant Pattnaik, Jay Kim  
Dept. of Mechanical Engineering  
University of Cincinnati





# What is HAVS

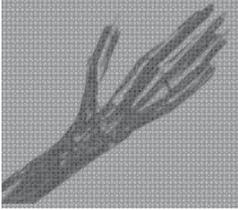
## Hand–Arm Vibration Syndrome

- Excessive vibration from Hand Tool causes MSD
- Musculoskeletal
- Sensorineural
- Vasospastic

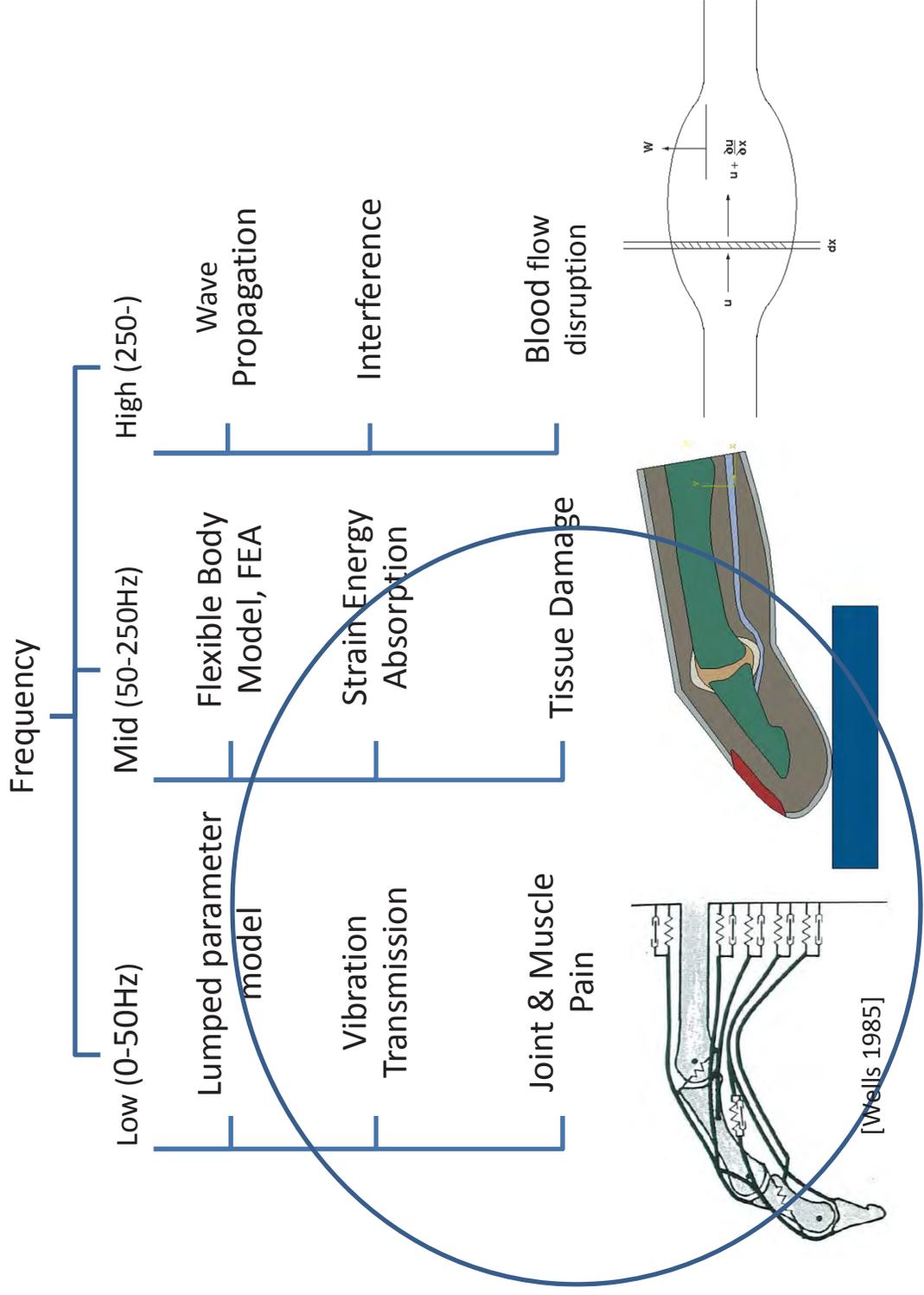


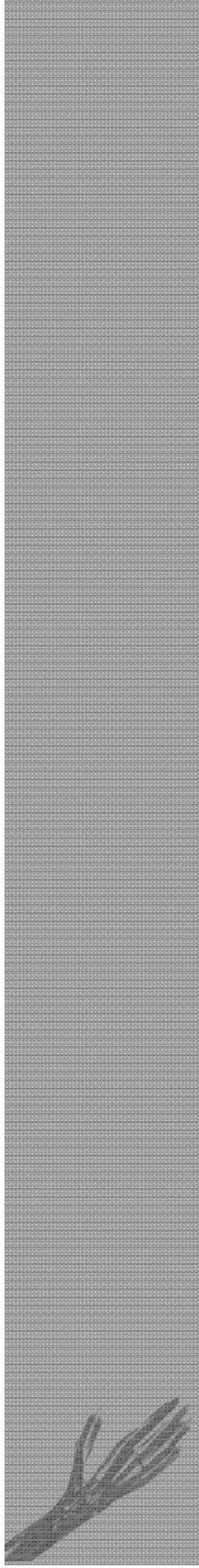
Raynaud's disease  
(blanching, numbness, pain)  
affects motor function





# Modeling Techniques

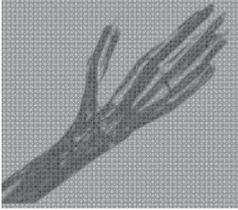




# Modeling | Lumped Parameter

Kinematic Model



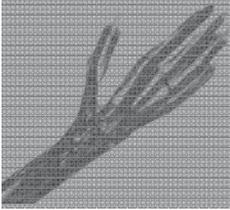


# LifeMOD

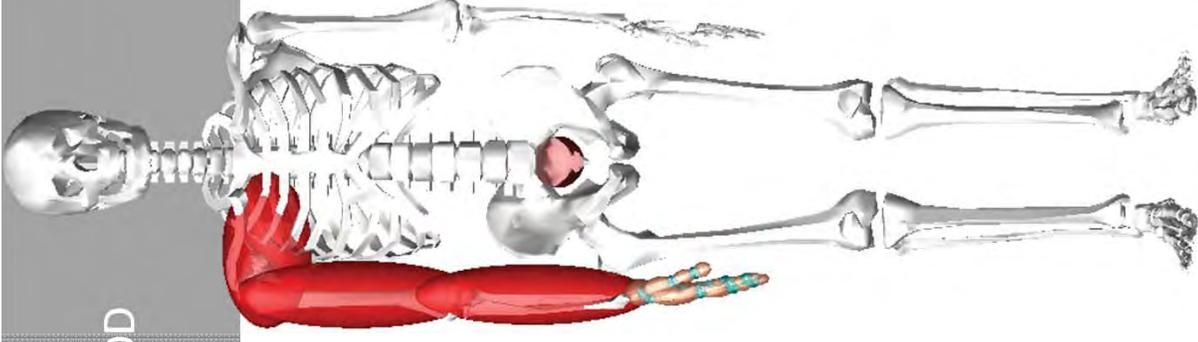
A plug-in of ADAMS

- plug-in module to the ADAMS physics engine.
- Human models can be combined with any ADAMS model for full dynamic interaction.
- Additional plug-ins – e.g. KneeSIM, NeckSIM - are available through LifeMOD.





# HandsIM A plug-in of LifeMOD



LifeMOD 2008.0.0  
File Edit View Build Simulate Review Settings Tools Help

World

Main Toolbox

View Control

Increment 30.0

Render

Grid

Depth

Icons

LifeMOD 2008.0.0  
Segments Create Base Segment Set Automated Tut

World Model Name World  
Human Body Name Albert  
Body Configuration Full Body Lower Body  
Anthropometric Database Library GeBOD

Weight (lbs) 77 Gender Male Female Child Non-Human  
Height (mm) 1778 Age (months) 288 Median

Create Body Measurement Table Apply  
Delete Existing Model  
Create Human Segments Apply

STATUS -> ADJUST THE VISUALIZATION PARAMETERS

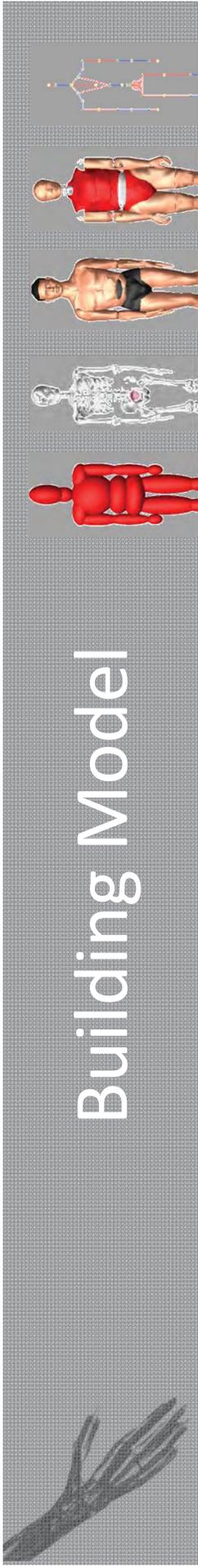
LifeMOD Display Toolbox

Active Body Isaac Units -> MKKS Move Tools Move Whole Body  
Body Body CM Tracker on/off Joints Graphics on/off  
Tissues Muscles on/off all on/off Motion Matrix Set on/off  
Misc. Items Forces on/off

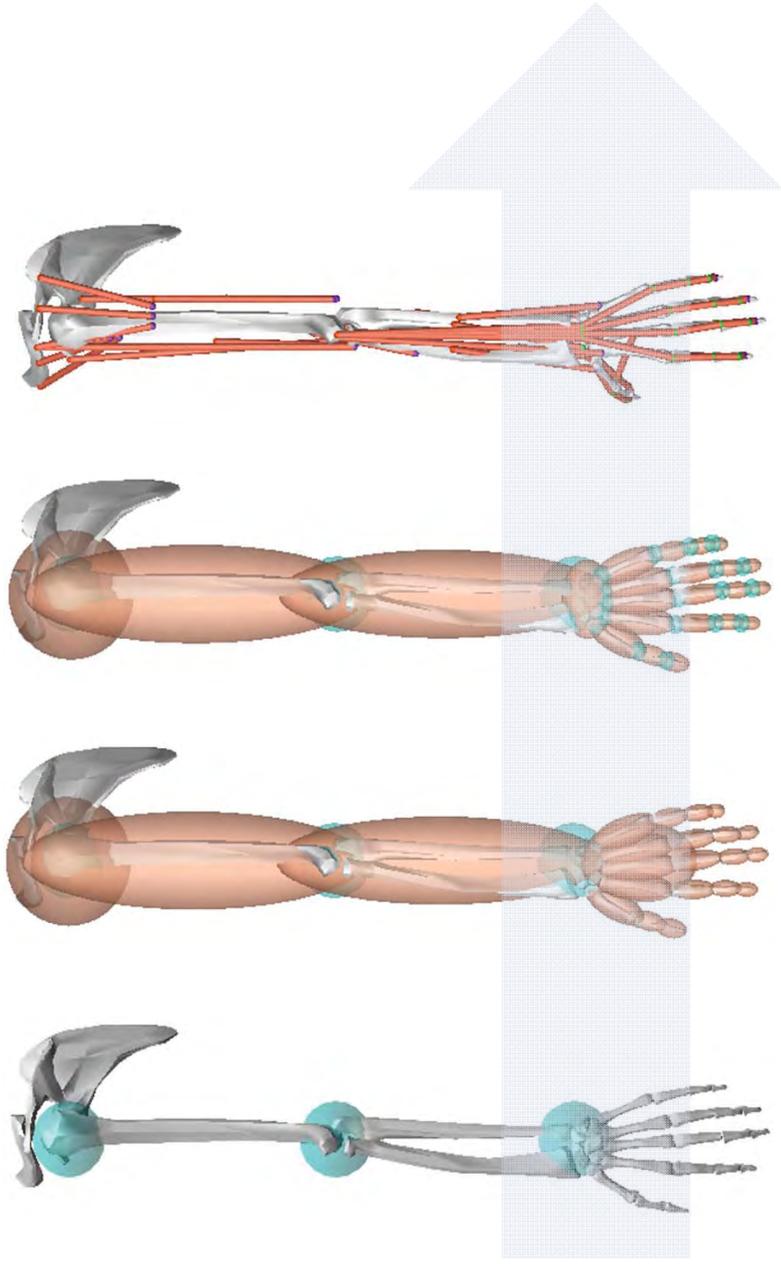
External Skin Ellipsoid Dummy none Internal Skeleton Stick none  
Transparency 0

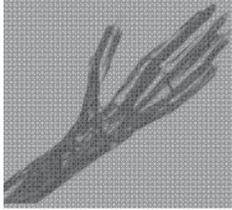
Draw Marker\_1 Erase Force\_1 Erase All Icons Default Part

LifeMOD - Automated Tutorial Control Panel  
Select Tutorial  
Select a tutorial from the list above



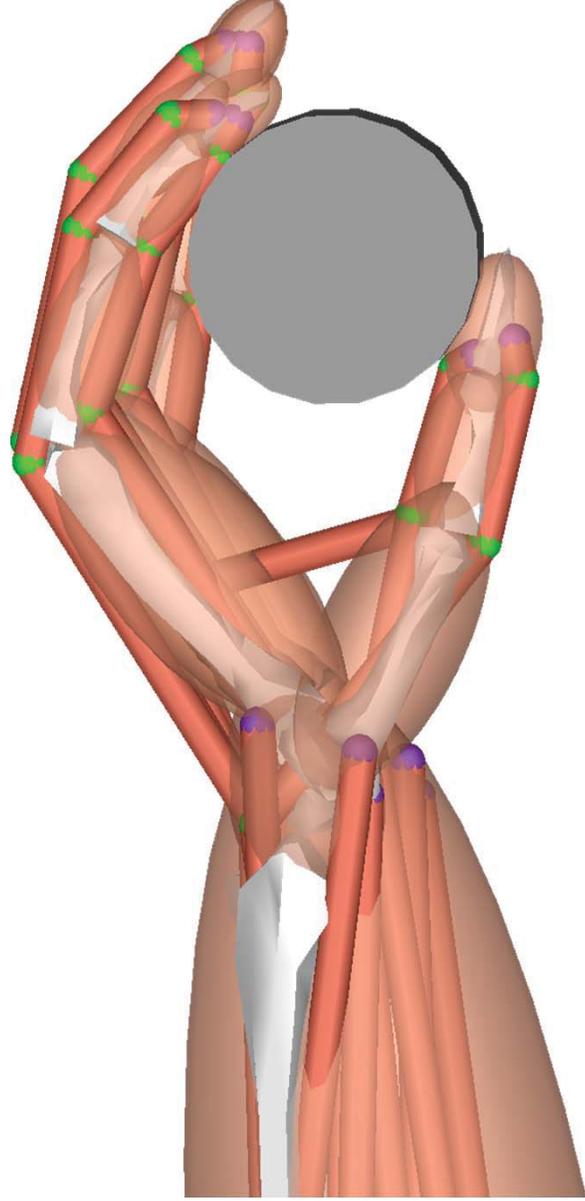
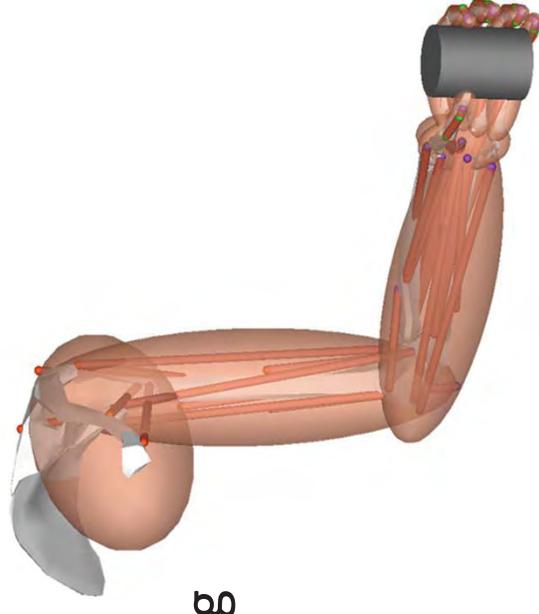
- Building a Model
  - Segments
  - Joints
  - Soft Tissues
- Muscle Model
  - Passive Modeling
  - Active Modeling



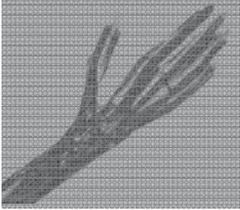


# Kinematic Modeling

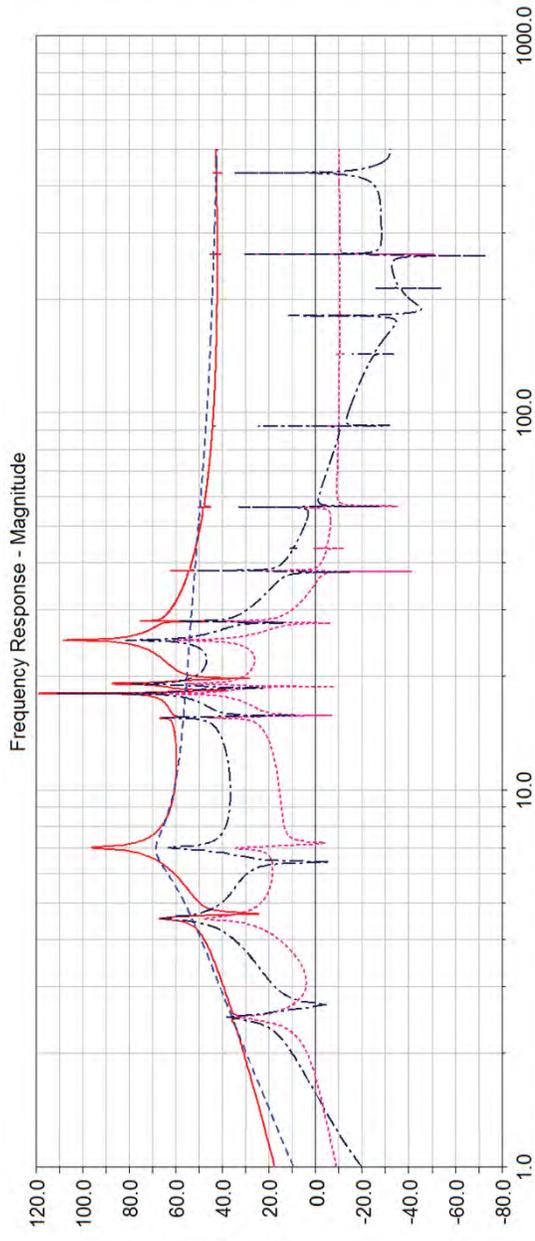
- Accurate geometry/mass properties
- 50<sup>th</sup> percentile human male attributes
- Tri-axial stiff joints, muscle with tissue wrapping
- Tension only muscle and “tone” defined



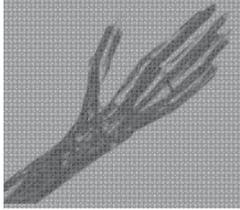
- Posture prediction
- Pre-load estimation



# Results: Frequency Response



Joint 12 (red) vs. elbow joint (magenta) vs. wrist (blue)  
z- accelerations upon input acceleration of  $1m/s^2$  at tip of cm of index finger.



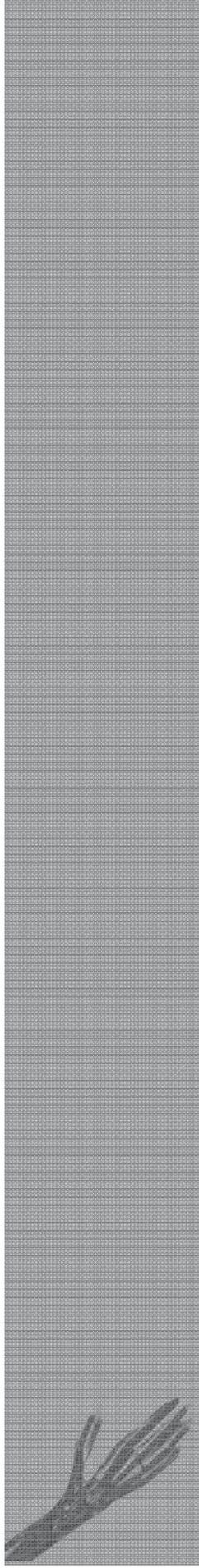
## Assumptions/Issues of Lumped Model

### **Assumptions – Lumped Parameter based Model:**

- Predefined degrees of freedom
- Linearity, non-viscous parameters
- Hand-tool rigid body based (only force and displacement)
- Assuming small displacements at the handle location, the dynamic response of the hand-arm system is considered to be uncoupled along its three orthogonal directions. ISO 8727

### **Issues:**

- High static deflections
- Lower natural frequencies with less mass and stiffness values in the parameters
- Dissipative property and other nonlinear behavior cannot be seen.

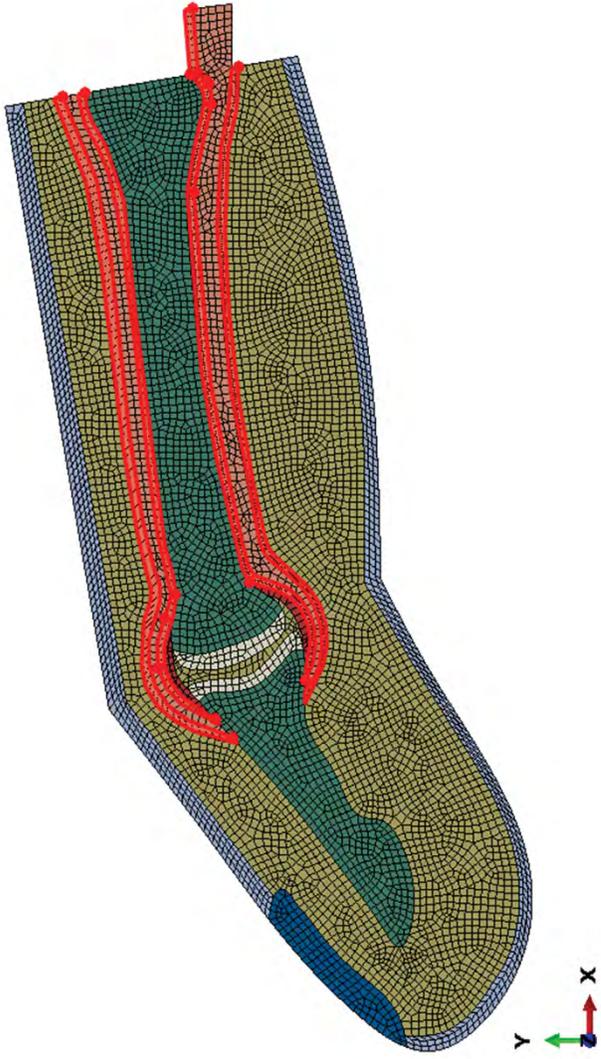
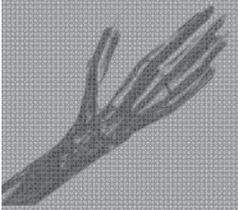


# Modeling | Flexible Body

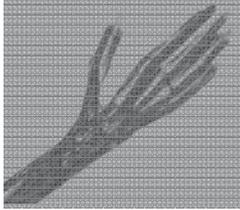
(Finite Element)



# Finite Element Model

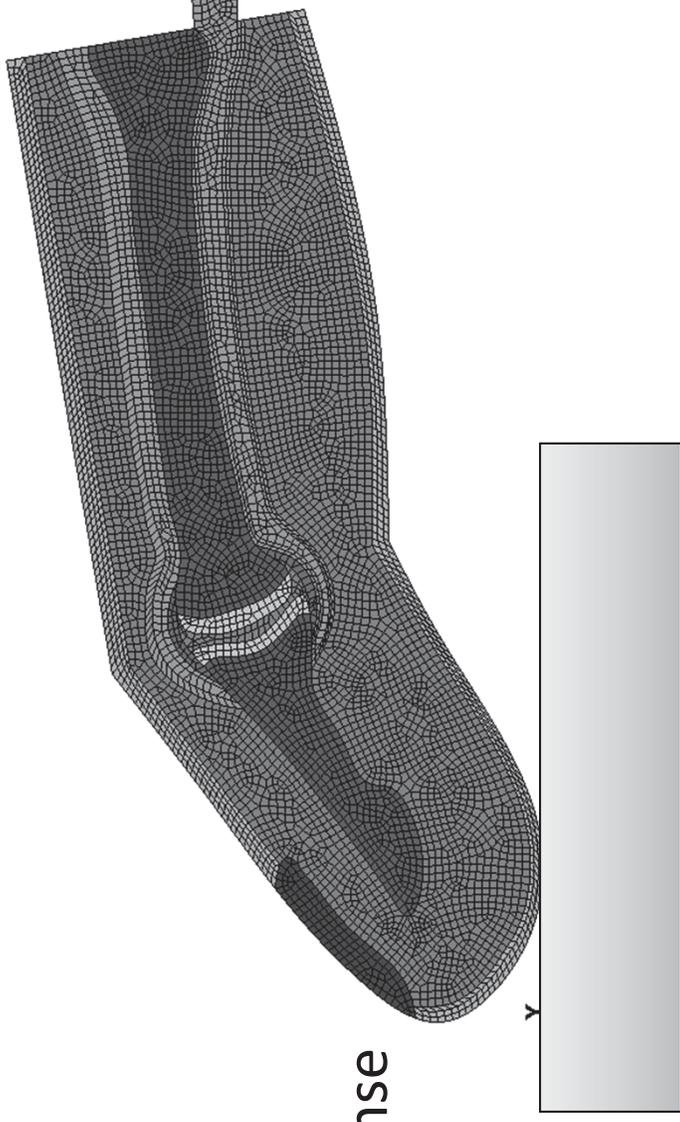


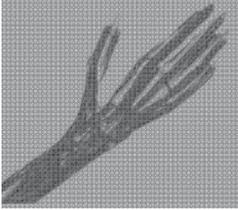
- Bone
- Soft Tissue
- Skin
- Nail
- Tendon
- Synovial Fluid
- Cartilage
- Ligament
- Sheath



# Finite Element Model

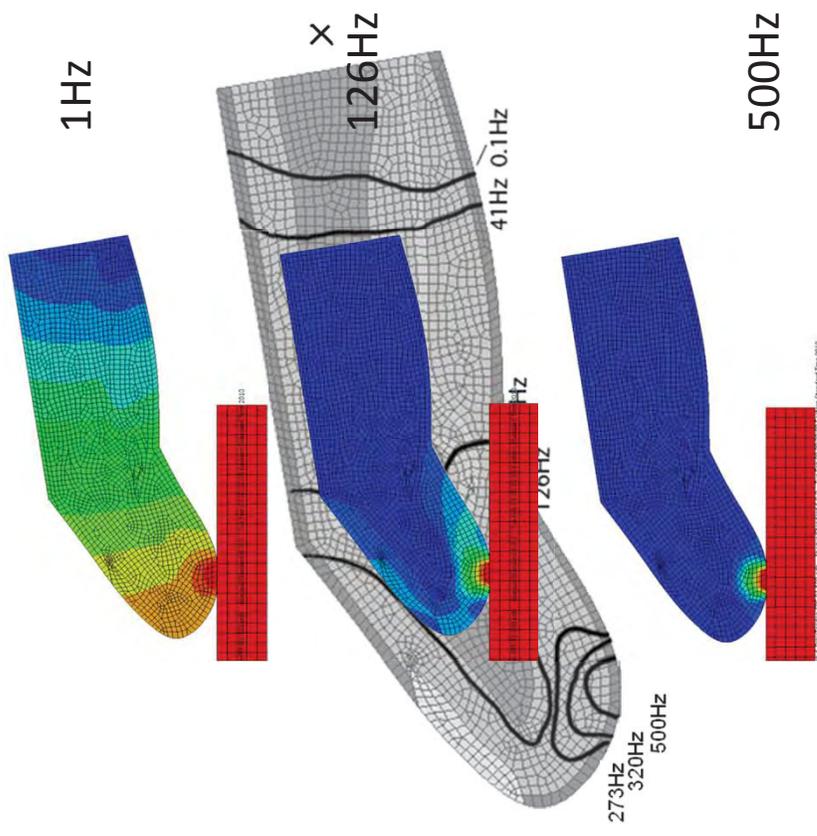
- Pre-loaded tendon
- Static deflection
- Dynamic simulation
- Modal Extraction
- High frequency response

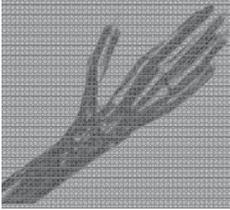




# Results: Dynamic response

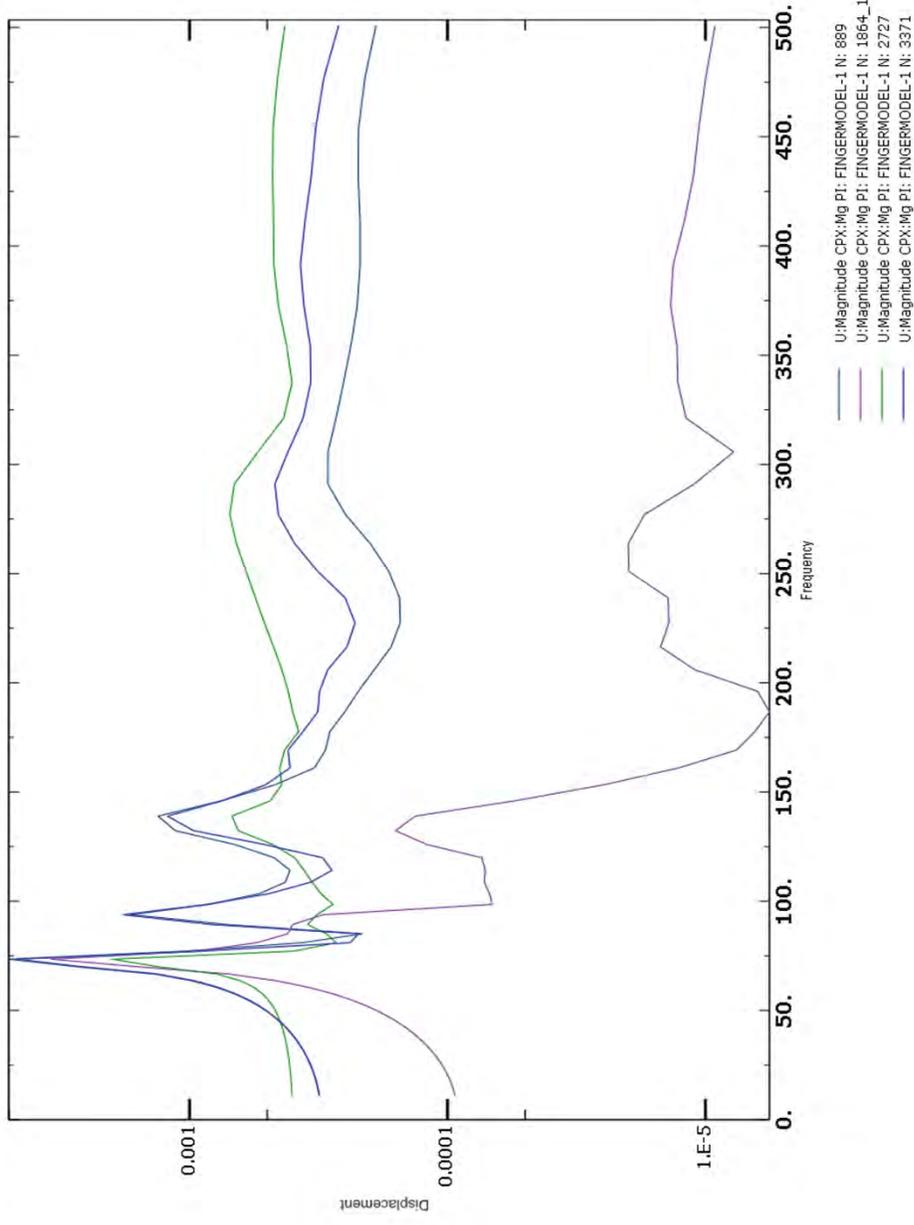
- Frequency response
- Stress/Strain evaluation
- Localized behavior with higher frequency

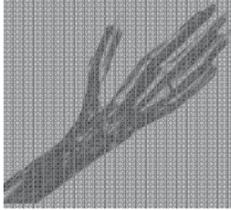




# Results: Frequency Response

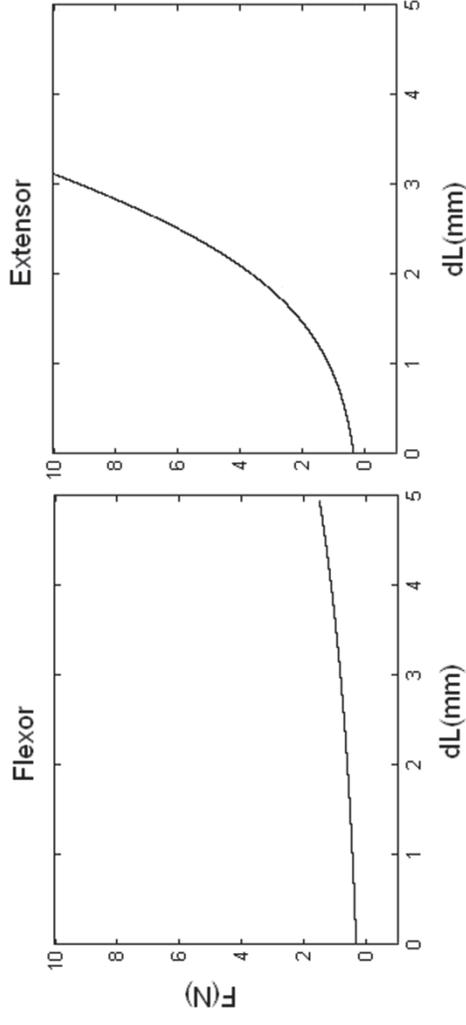
Mode	Freq(Hz)	Mode	Freq(Hz)
1	62.86	11	192.26
2	73.69	12	196.72
3	92.04	13	206.72
4	107.43	14	214.26
5	128.86	15	220.78
6	134.83	16	226.78
7	142.45	17	230.38
8	159.85	18	235.70
9	168.29	19	241.83
10	179.34	20	243.39

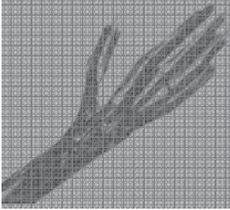




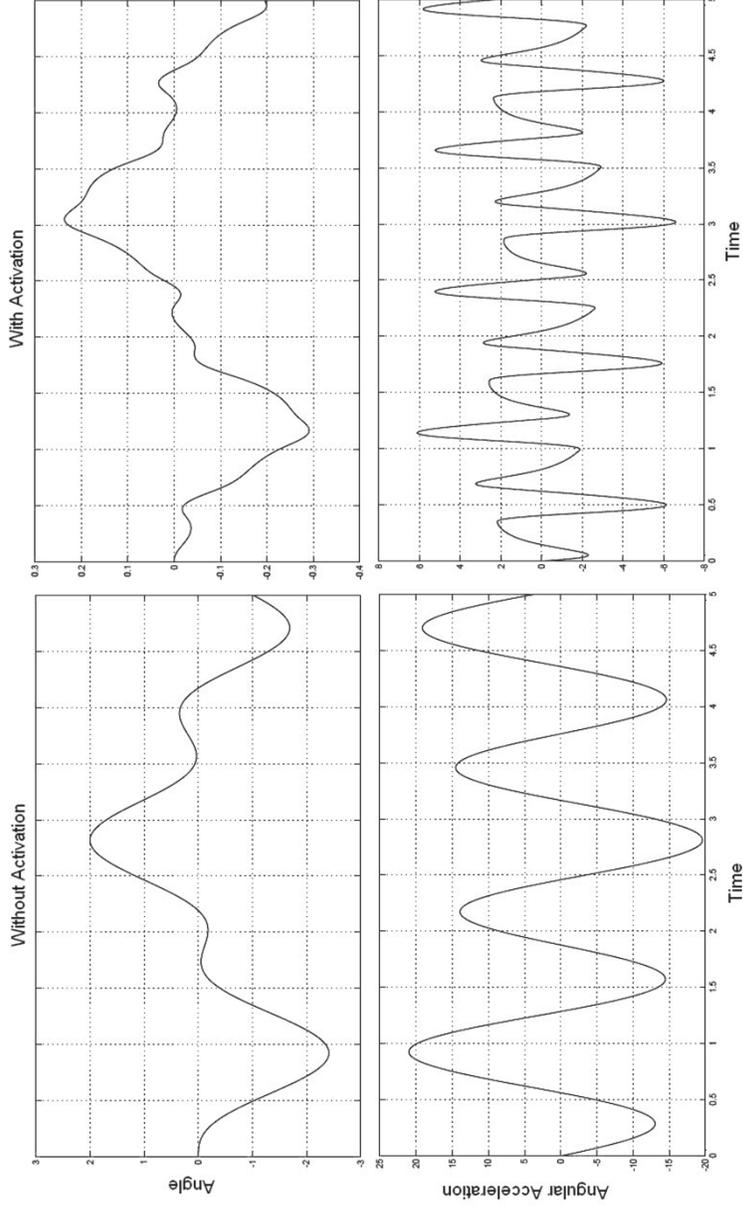
## Observation 1/2: Relative Muscle Contribution

- Nonlinear response
- Flexor four times size of Extensor
- Short and long range force output
- Static vs. Dynamic counterbalance

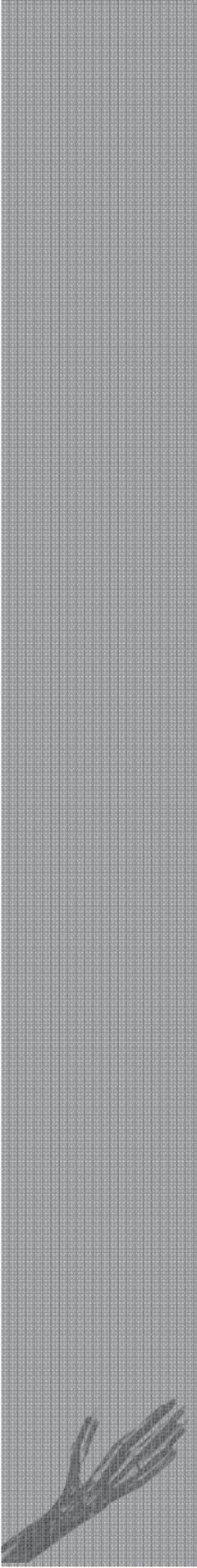




# Observation 2/2: Activated Response



Distal Interphalangeal (DIP) Joint



# Coupled Modeling | Rigid + Flexible

Kinematic + Finite Element

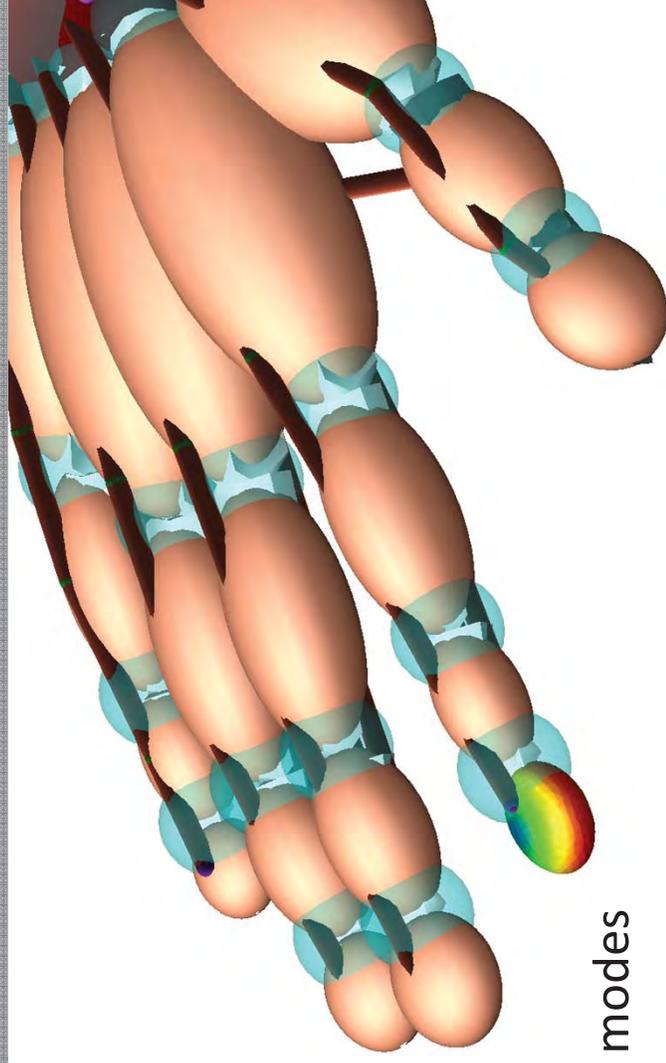
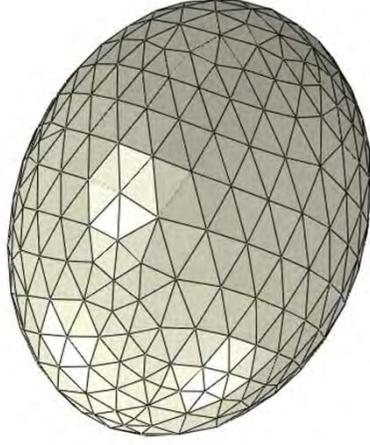


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Bringing Simulation to Life™

+



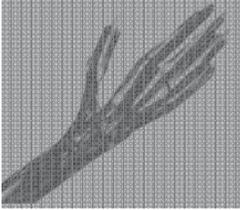
# Rigid-Flexible Coupled Approach



## Steps

- LifeMOD – export IGES
- ABAQUS – substructure – extract modes
- Run Macro - Mode Neutral File
- Import LifeMOD replace rigid with Flex

Stress/Strain Contour on a Flexible part

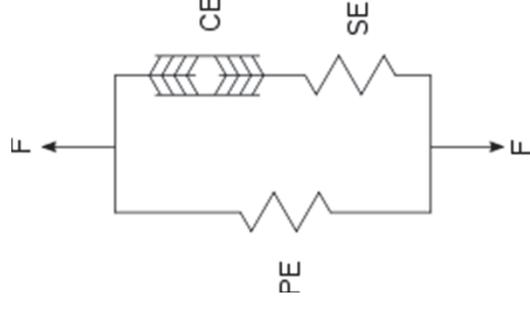


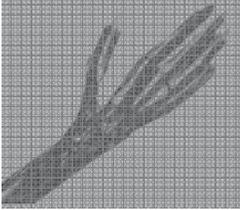
## Discussion 1/3

- Damping can occur by three mechanisms:
  - passive damping properties of elastic tissue and tool surface
  - force-velocity properties of active muscle
  - well-timed activation pulses that occur when a muscle is in the lengthening phase of the vibration.  
( Low freq )

- High freq – passive spring series element

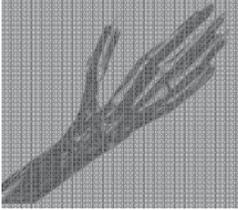
(Hill's model)





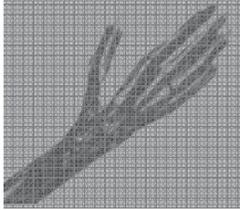
## Discussion 2/3

- Extrinsic (Flexor) creates static grip force.
- dynamic load –Extensor & Intrinsic
- Interphalangeal joint stabilized with co-activation
- Transmission of vibration increases with co-contraction.
- Higher grip force -> higher impedance and higher resonance (muscles stiffened)
- Higher muscle force higher stiffness lesser is the deformation needed to absorb same energy



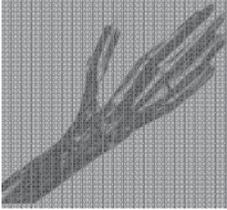
## Discussion 3/3

- Under dynamic loading friction coefficient of articular cartilage reduces
- Fast Dynamic load – elastic behavior (approx.)
- Tougher the component and the greater the volume more strain energy it is likely to absorb.
- Capacity of absorbing strain energy
  - Highest - Tendon 65 times of muscle
  - Bone 55 times of muscle
  - Lowest - Muscle



## Conclusion/Future Work

- Improve Combined approach (Kinematic and FE)
- High frequency -> faster Type II (vs. Slower Type I)
- Rest of the segments of hand
- Contact stress evaluation
- Fatigue model



# Thank You

## Acknowledgements

- Advisor – Dr. Jay Kim
- Dr. Rupak Banerjee
- Dr. Ren Dong & NIOSH -Morgantown Team
- P&G/UC – Simulation Center
- This research study was (partially) supported by the National Institute for Occupational Safety and Health Pilot Research Project Training Program of the University of Cincinnati Education and Research Center Grant #T42/OH008432-05.



**University of Cincinnati  
11th Annual  
Pilot Research Project  
Symposium  
October 14-15, 2010**

**Main Menu**

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The National Institute for Occupational Safety and Health.  
(NIOSH) Grant #: T42/OH008432-05

- ◆ **Welcome and Opening Remarks**
- ◆ **Keynote Speakers**
- ◆ **Podium Presentations**
- ◆ **Poster Presentations**
- ◆ **Video Montage of the 11th Annual PRP Symposium**
- ◆ **Participating Universities**
- ◆ **Steering Committee Members**
- ◆ **Acknowledgements**
- ◆ **Problems Viewing the Videos**

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