

**12th Annual
2011 Pilot Research Project
(PRP) Symposium**

Thursday, Oct. 13, 1 pm-5:15 pm
Friday, Oct. 14, 8 am-12:15 pm
Kehoe Auditorium, Kettering Laboratory

**Supported by NIOSH Grant
#T42-OH008432**

Effect of Aging on Human Postural Control: A Predictive Modeling Approach

Carson Willey

Amit Shukla

Renu Sah

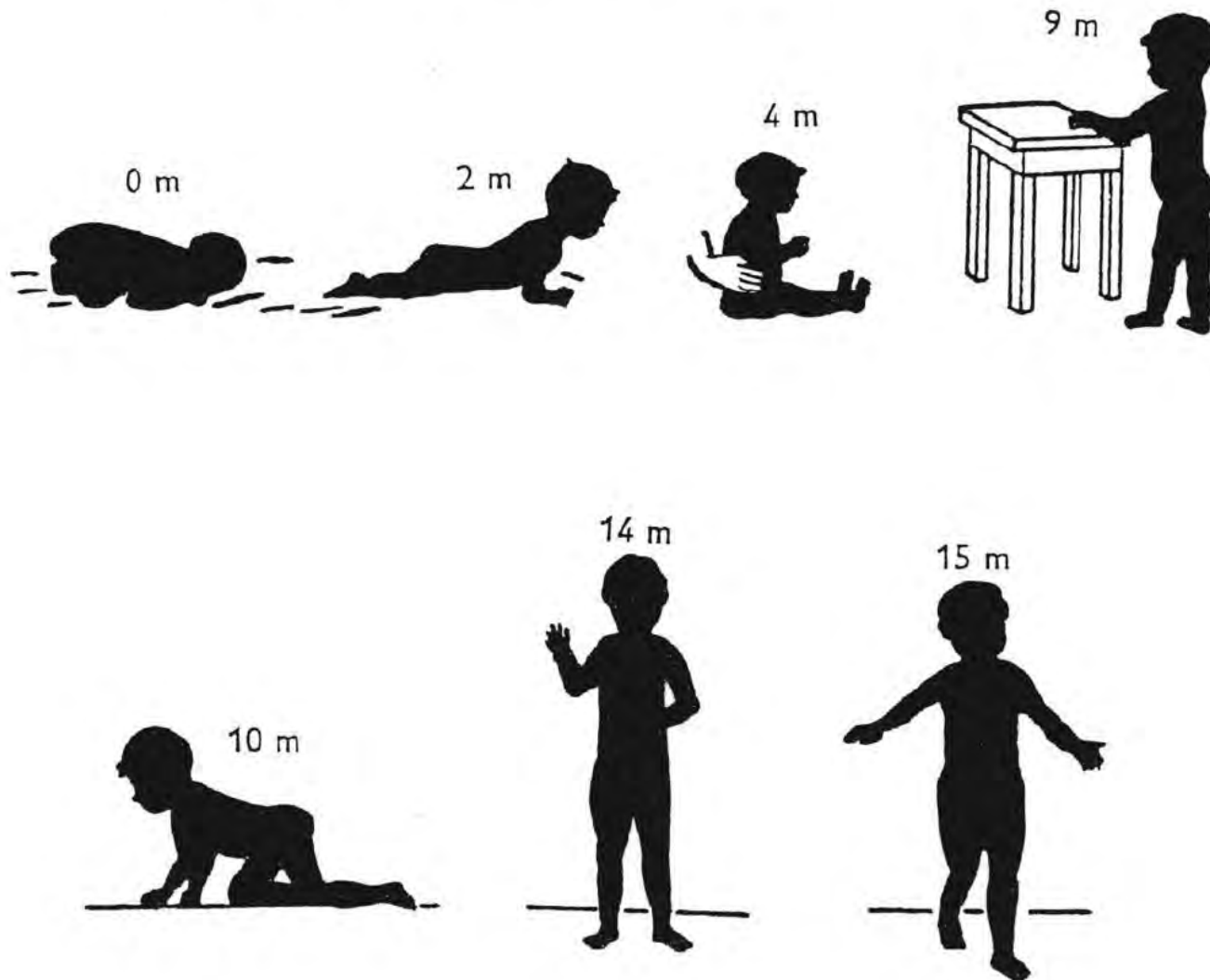


**MIAMI
UNIVERSITY**
OXFORD OHIO

Outline

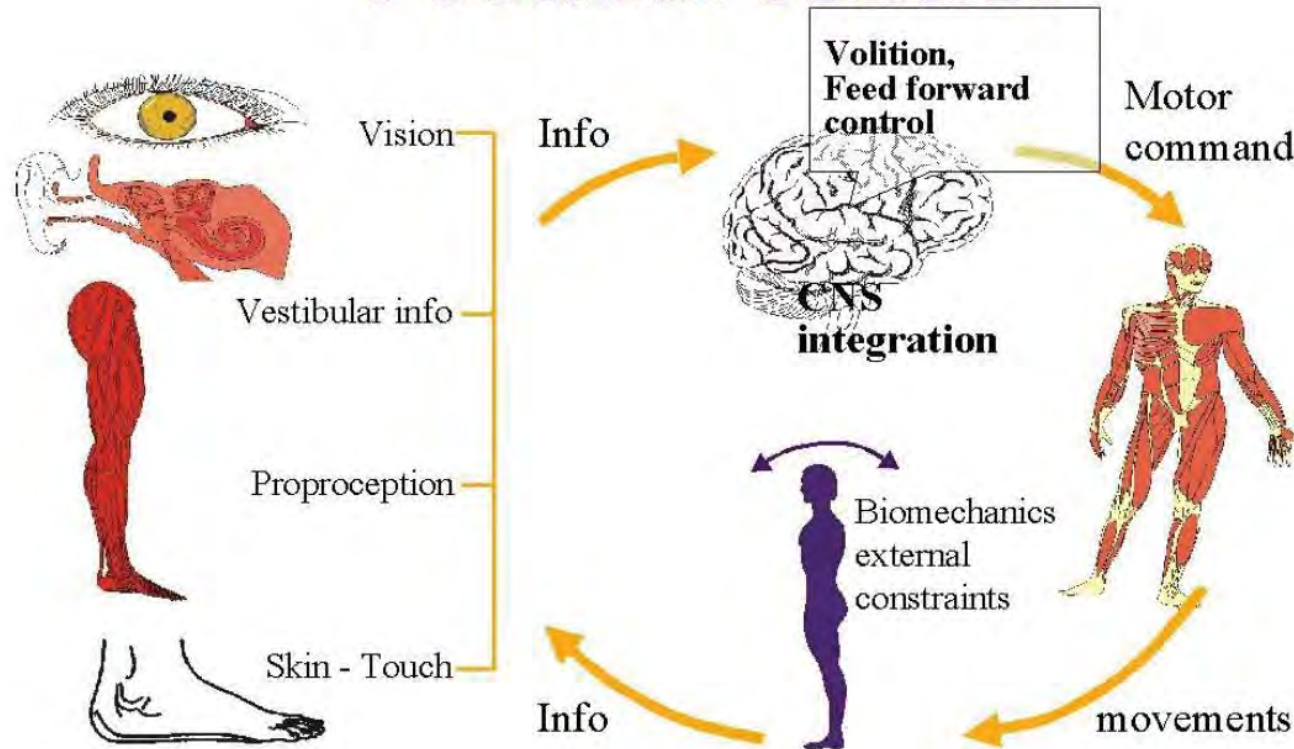
- Balance and Aging
- Modeling Balance: Dynamics and Control
- L-2 Norm as a balance metric
- Parametric Studies
- Results and Discussion
- Future Work

Balance and Posture



Human Postural Control: Why?

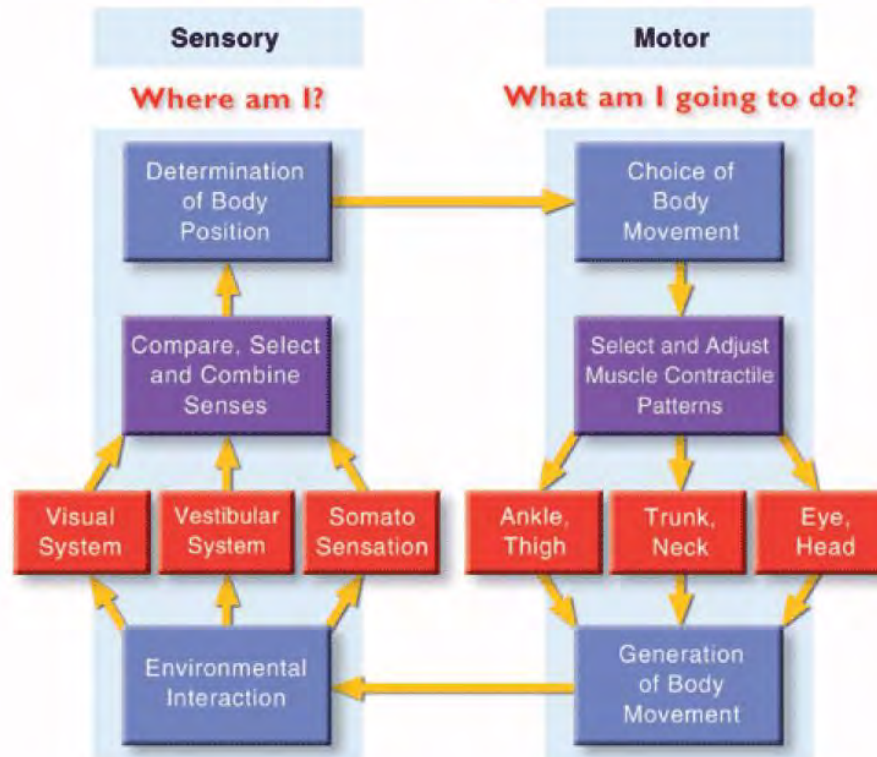
Postural control



Courtesy: Swedish Medical Research Council

Human Postural Control

Balance Control



Jacobson GP, Newman CW, Kartush JM (1993). *Handbook of Balance Function Testing*. Mosby Year Book, St Louis.

Human Postural Control

Imbalance could be due to:

- cardiovascular dysfunction,
- visual disorientation,
- inadequate limb proprioception,
- vestibular signals or dysfunction.

Complex Nature of Balance Problems

Human Postural Control: Medical Causes

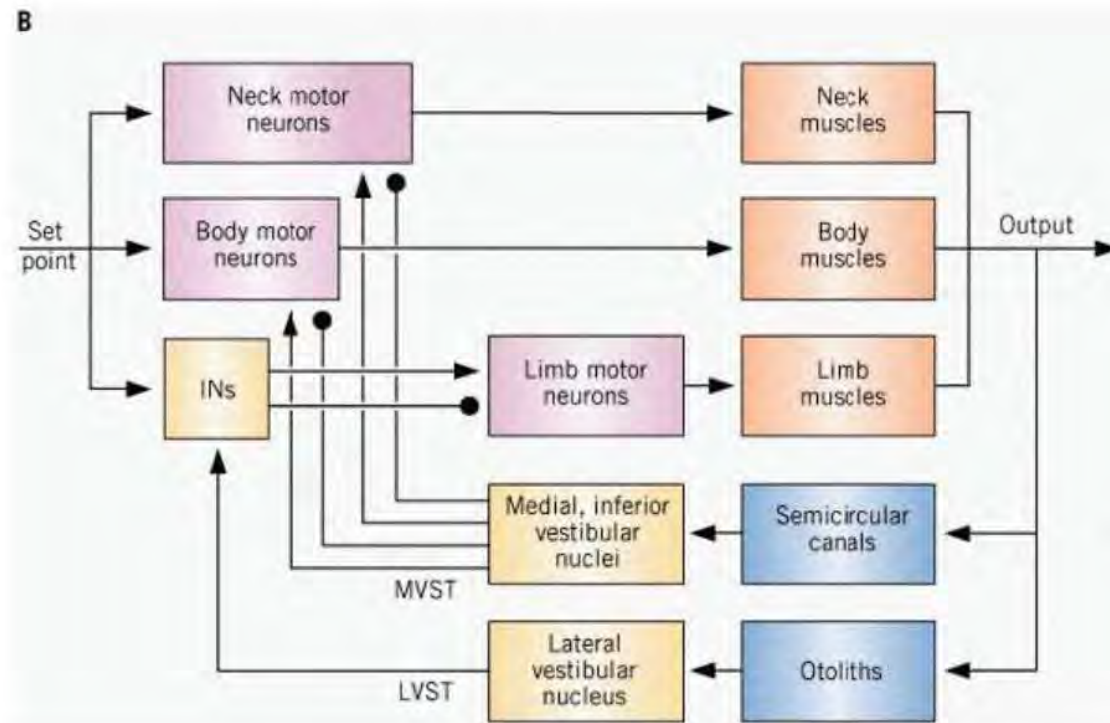
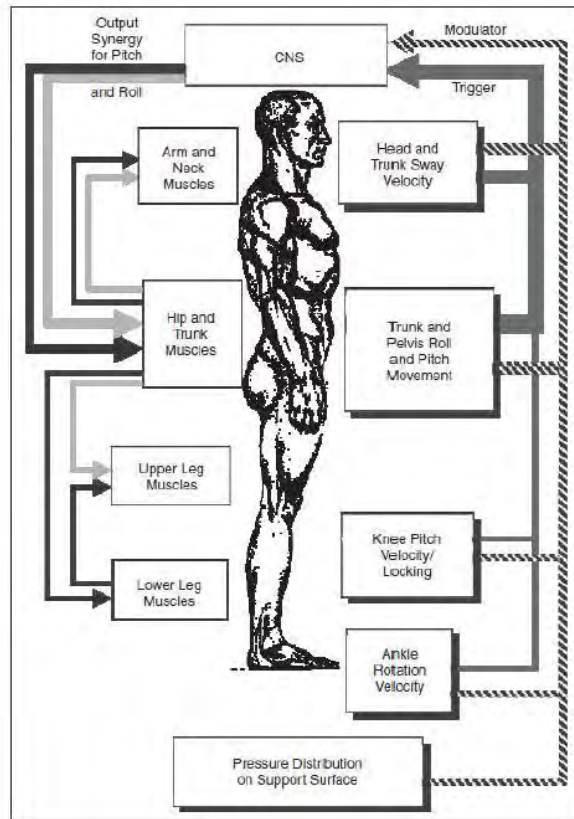
- Aging and Balance Dysfunction
 - Parkinson's Disease
 - Accumulated Injuries
 - Ear infections
 - Diabetes
 - Others



Whether balance disorders result from combinations of subtle problems or obvious disease, clinical studies indicate that elderly fallers are different from their healthy age-matched counterparts and require medical treatment to maintain their functional independence and quality of life.

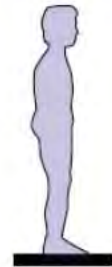
Dynamics and Control

Multiple sensor-multiple inputs



Dynamics and Control

Dynamics posturography with sensory condition number (κ)



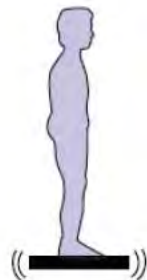
$\kappa = 1$:
Normal



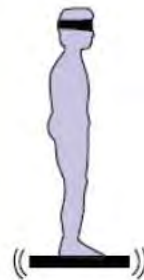
$\kappa = 2$:
Eyes closed



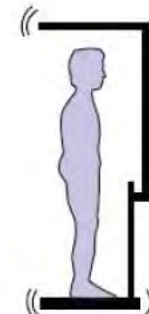
$\kappa = 3$:
Vision sway-ref



$\kappa = 4$:
Platform
sway-ref



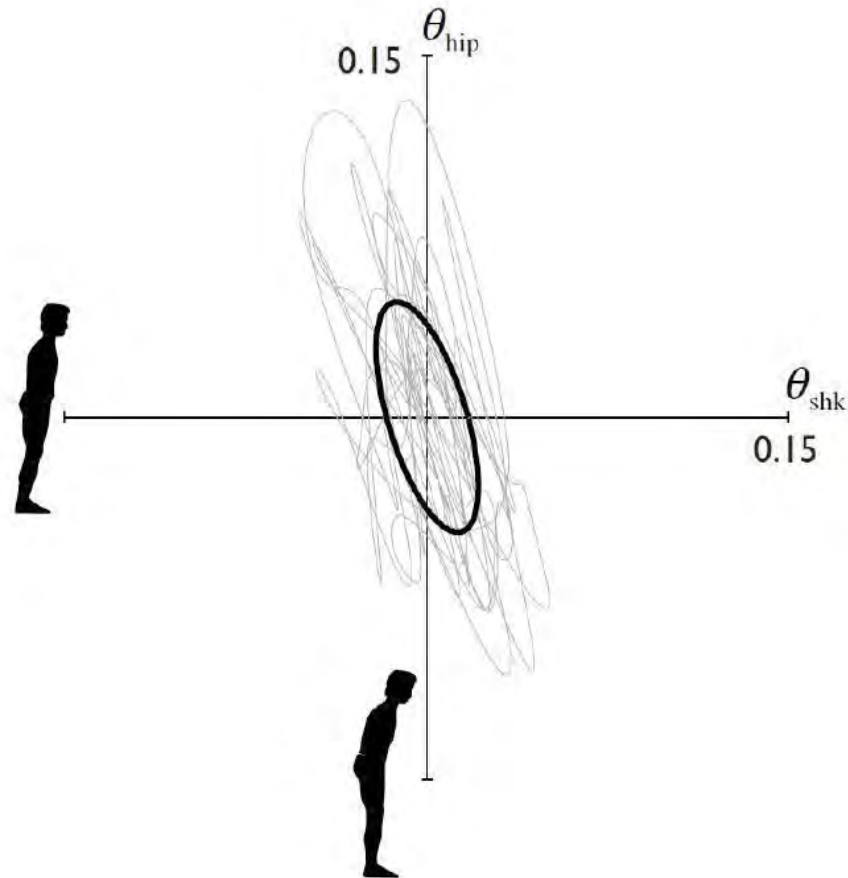
$\kappa = 5$:
Eyes closed
Platform sway-ref



$\kappa = 6$:
Vision sway-ref
Platform sway-ref

Dynamics and Control

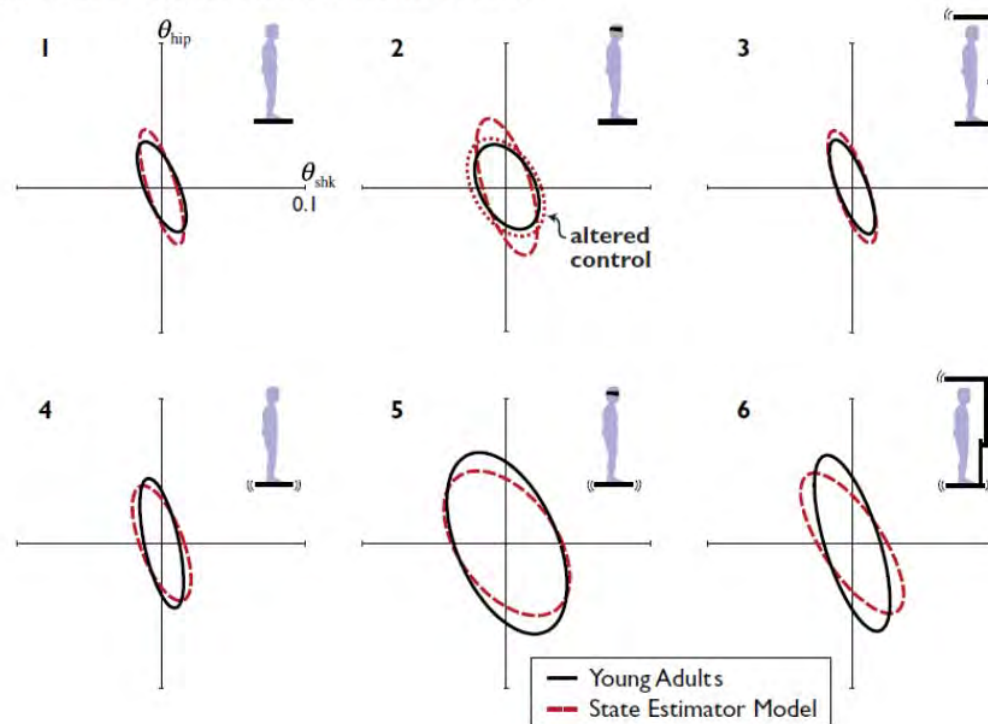
Covariance data: shank angle vs. hip angle



Dynamics and Control

Covariance data: shank angle vs. hip angle

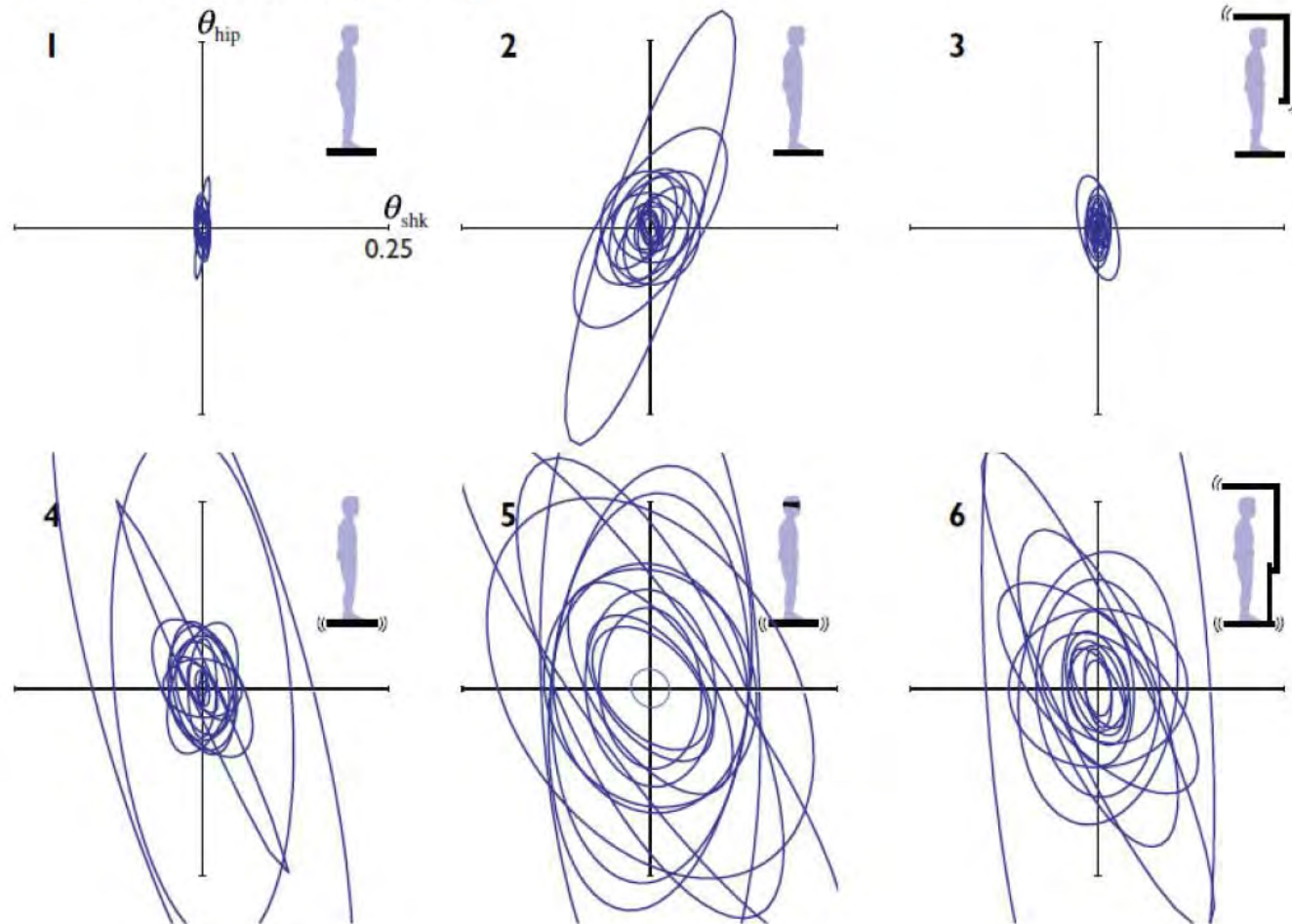
(a) State Estimator Model of Normal Posture



Kuo A D 1995 An optimal control model for analyzing human postural balance *IEEE Trans. Biomed. Eng.* **42** 87–101

Dynamics and Control

Older Adult Subjects (N = 15)



The One Degree of Freedom Model

Parameter	Value	Units
m	80	kg
g	9.81	m/s ²
h	1	m
K	.25 mgh	N/rad
B	4	N/rad * s
P	.8 mgh	N/rad
D	14	N/rad * s
a	-.4	rad/s/rad
r	.004	

$$I\ddot{\theta} = mgh \sin(\theta) - T$$

$$T = K\theta + B\dot{\theta} + P\theta_{\Delta} + D\dot{\theta}_{\Delta}$$

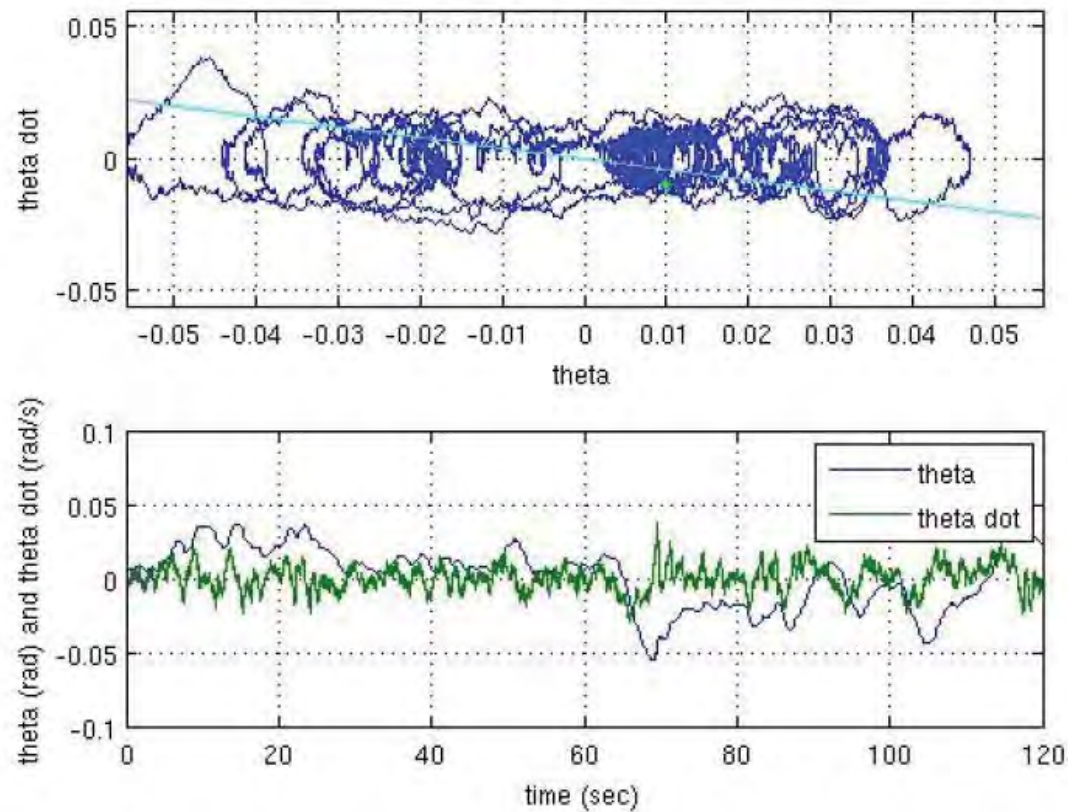
$$\theta_{\Delta} = \theta(t - \tau)$$

$$\dot{\theta}_{\Delta} = \dot{\theta}(t - \tau)$$

$$\sqrt{\dot{\theta}_{\Delta}^2 + \theta_{\Delta}^2} < r \text{ and } \theta_{\Delta}(\dot{\theta}_{\Delta} - a\theta_{\Delta}) > 0$$

[1] Y. Asai, Y. Tasaka, K. Nomura, T. Nomura, and M. Casadio, "A model of postural control in quiet standing: Robust compensation of delay-induced instability using intermittent activation of feedback control," PLoS ONE, vol. 4, no. 7, 2009.

One DOF Model Output



The Two Degree of Freedom Model

Pendulum Dynamics

$$\begin{aligned} \ddot{\theta}_1(2\alpha - (\delta^2)/(2\beta) \cos(\theta_1 - \theta_2)^2) &= -(\delta^2)/(2\beta) \dot{\theta}_1^2 \sin(\theta_1 - \theta_2) \cos(\theta_1 - \theta_2) \\ &\quad -(\delta\zeta)/(2\beta) \sin(\theta_2) \cos(\theta_1 - \theta_2) - \delta \dot{\theta}_2^2 \sin(\theta_1 - \theta_2) + \gamma \sin(\theta_1) - T_1 \\ \ddot{\theta}_2(2\beta - (\delta^2)/(2\alpha) \cos(\theta_1 - \theta_2)^2) &= (\delta^2)/(2\alpha) \dot{\theta}_2^2 \sin(\theta_1 - \theta_2) \cos(\theta_1 - \theta_2) \\ &\quad -(\delta\gamma)/(2\alpha) \sin(\theta_1) \cos(\theta_1 - \theta_2) + \delta \dot{\theta}_1^2 \sin(\theta_1 - \theta_2) + \zeta \sin(\theta_2) - T_2 \end{aligned}$$

Constants

$$\alpha = (m_1 l_1^2)/8 + (m_2 l_1^2)/2 + I_1/2$$

$$\beta = (m_2 l_2^2)/8 + I_2/2$$

$$\gamma = (g m_1 l_1)/2 + g m_2 l_1$$

$$\zeta = (g m_2 l_2)/2$$

$$\delta = (m_2 l_2 l_1)/2$$

$$I_1 = (m_1 l_1^2)/12$$

$$I_2 = (m_2 l_2^2)/12$$

Controller Torques

$$\begin{aligned} T_1 &= K_1 \theta_1 + K_2(\theta_1 - \theta_2) + B_1 \dot{\theta}_1 + B_2(\dot{\theta}_1 - \dot{\theta}_2) + P_1 \theta_{1\Delta} + P_2(\theta_{1\Delta} - \theta_{2\Delta}) + D_1 \dot{\theta}_{1\Delta} \\ &\quad + D_2(\dot{\theta}_{1\Delta} - \dot{\theta}_{2\Delta}) + \sigma \eta \\ T_2 &= K_2(\theta_2 - \theta_1) + B_2(\dot{\theta}_2 - \dot{\theta}_1) + P_2(\theta_{2\Delta} - \theta_{1\Delta}) + D_2(\dot{\theta}_{2\Delta} - \dot{\theta}_{1\Delta}) + \sigma \eta \end{aligned}$$

$$\theta_{j\Delta} = \theta_j(t - \tau)$$

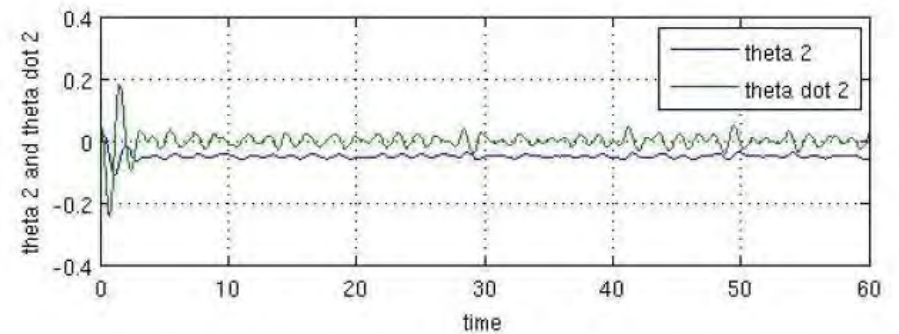
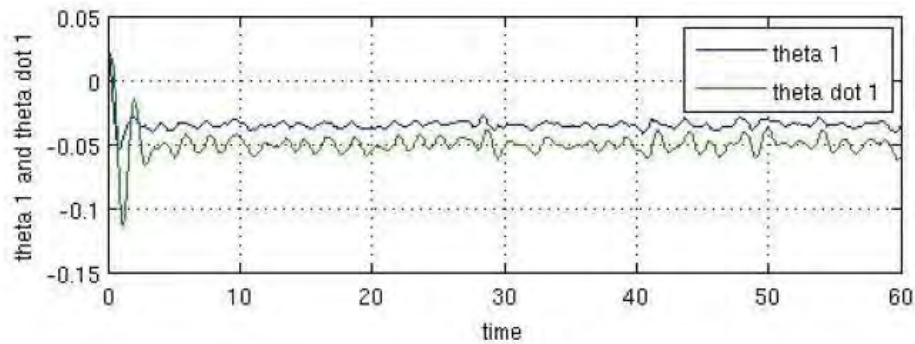
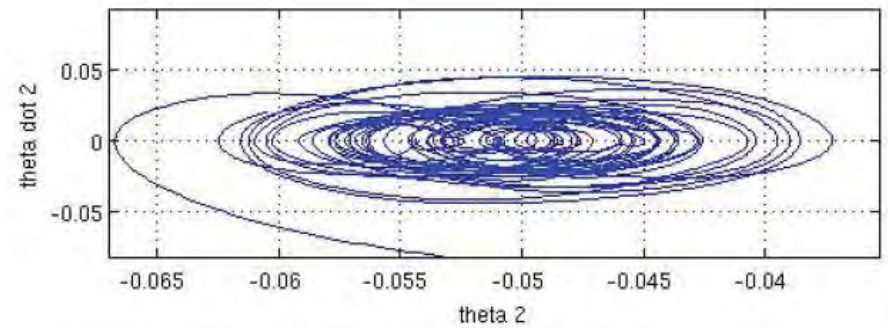
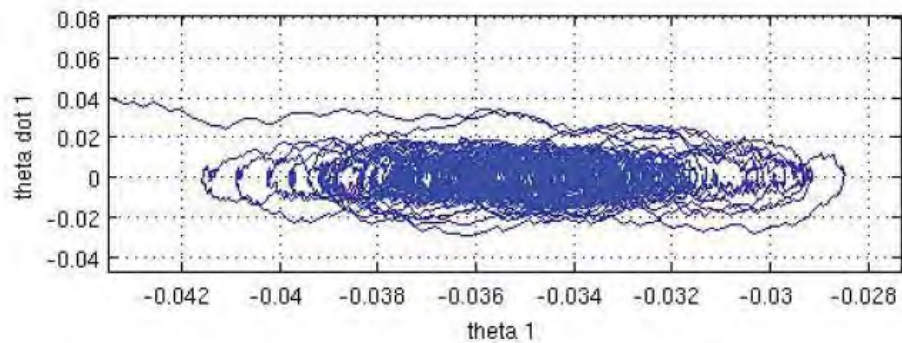
$$\dot{\theta}_{j\Delta} = \dot{\theta}_j(t - \tau)$$

Intermittent
Activation
Conditions

$$\sqrt{\dot{\theta}_{1\Delta}^2 + \theta_{1\Delta}^2} < r \text{ and } \theta_{1\Delta}(\dot{\theta}_{1\Delta} - a\theta_{1\Delta}) > 0$$

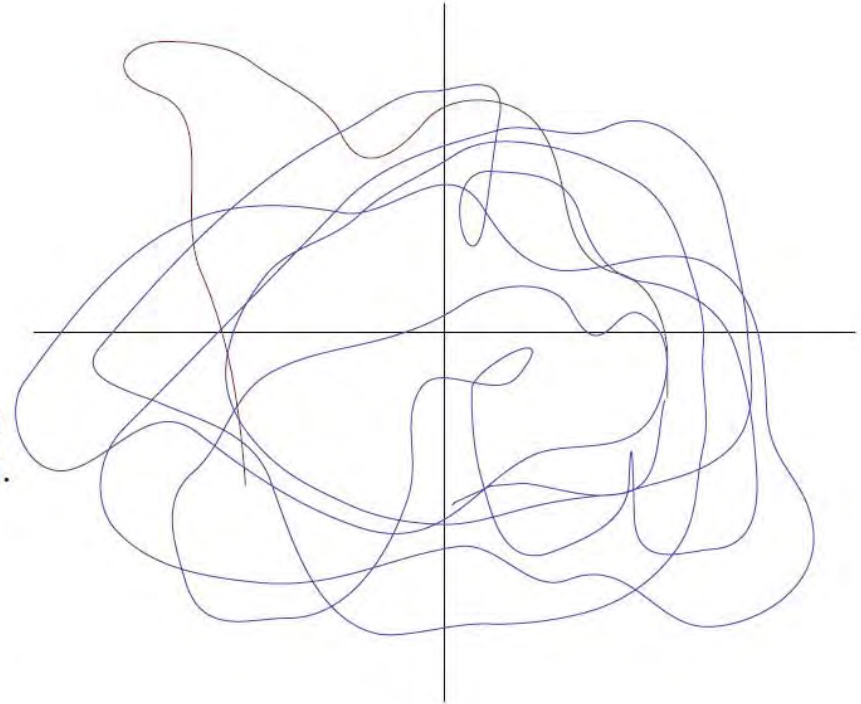
$$\begin{aligned} &\sqrt{(\dot{\theta}_{2\Delta} - \dot{\theta}_{1\Delta})^2 + (\theta_{2\Delta} - \theta_{1\Delta})^2} < r \text{ and} \\ &(\theta_{2\Delta} - \theta_{1\Delta})((\dot{\theta}_{2\Delta} - \dot{\theta}_{1\Delta}) - a(\theta_{2\Delta} - \theta_{1\Delta})) > 0 \end{aligned}$$

Two DOF Model Output



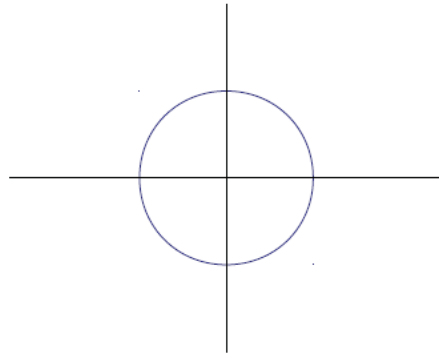
Average L₂ Norm Analysis

- As $t \rightarrow \infty$
- Case1 : Avg L₂ Norm < Ref L₂ Norm
- Case2 : Avg L₂ Norm \approx Ref L₂ Norm
- Case3 : Avg L₂ Norm > Ref L₂ Norm
- Ref L₂ is the average norm taken with respect to the delay history (red).
- Avg L₂ Norm is the same measure taken with respect to the projected curve (blue).

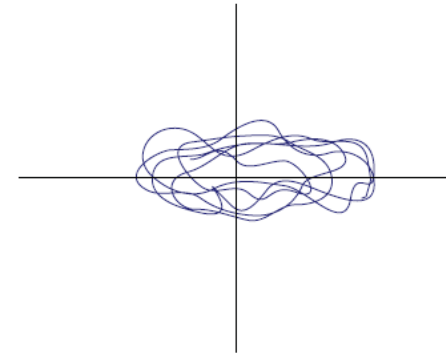


$$L_{2 \text{ avg}} = \frac{1}{N} \sum_{i=1}^N L_i \text{ where } L_i = \sqrt{x_i^2 + y_i^2}$$

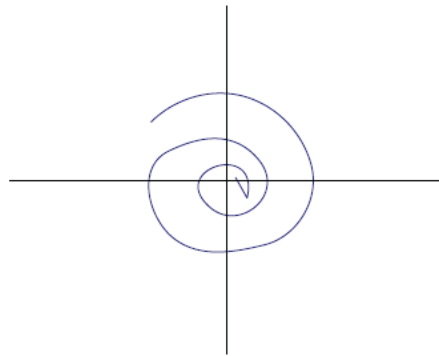
Average L_2 Norm Analysis



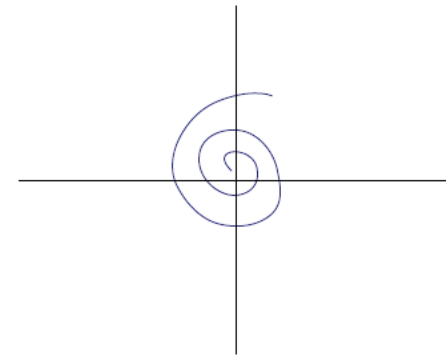
Case 2 : constant energy



Case 2 : realistic phase plot



Case 1 : Decreasing Energy

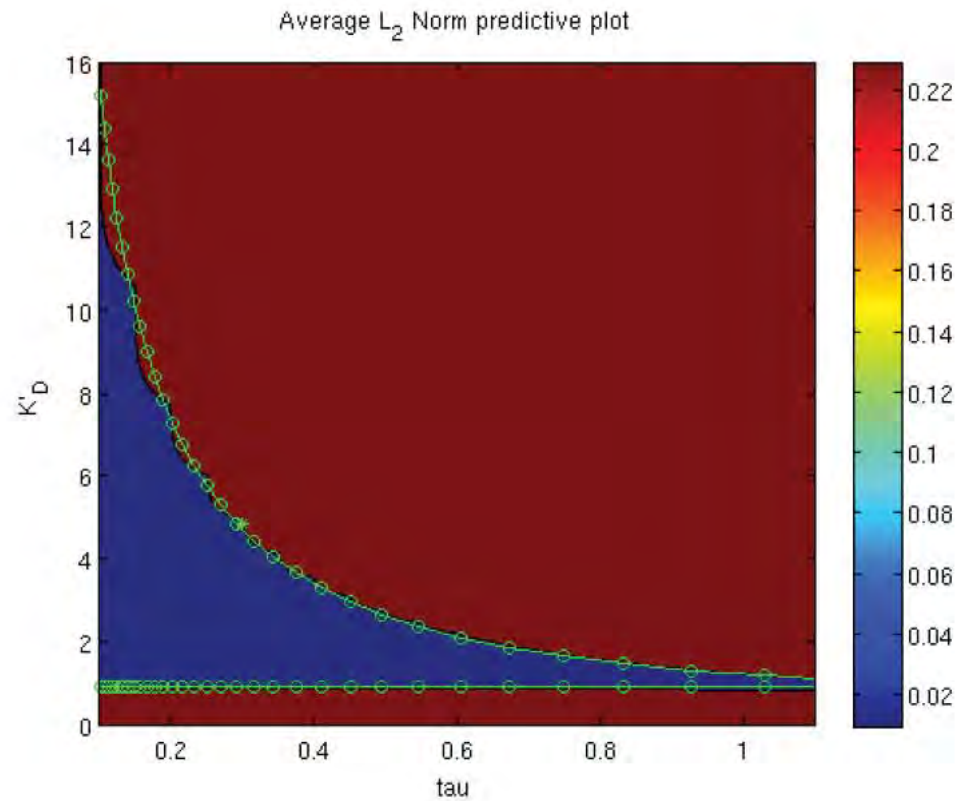


Case 3 : Increasing Energy

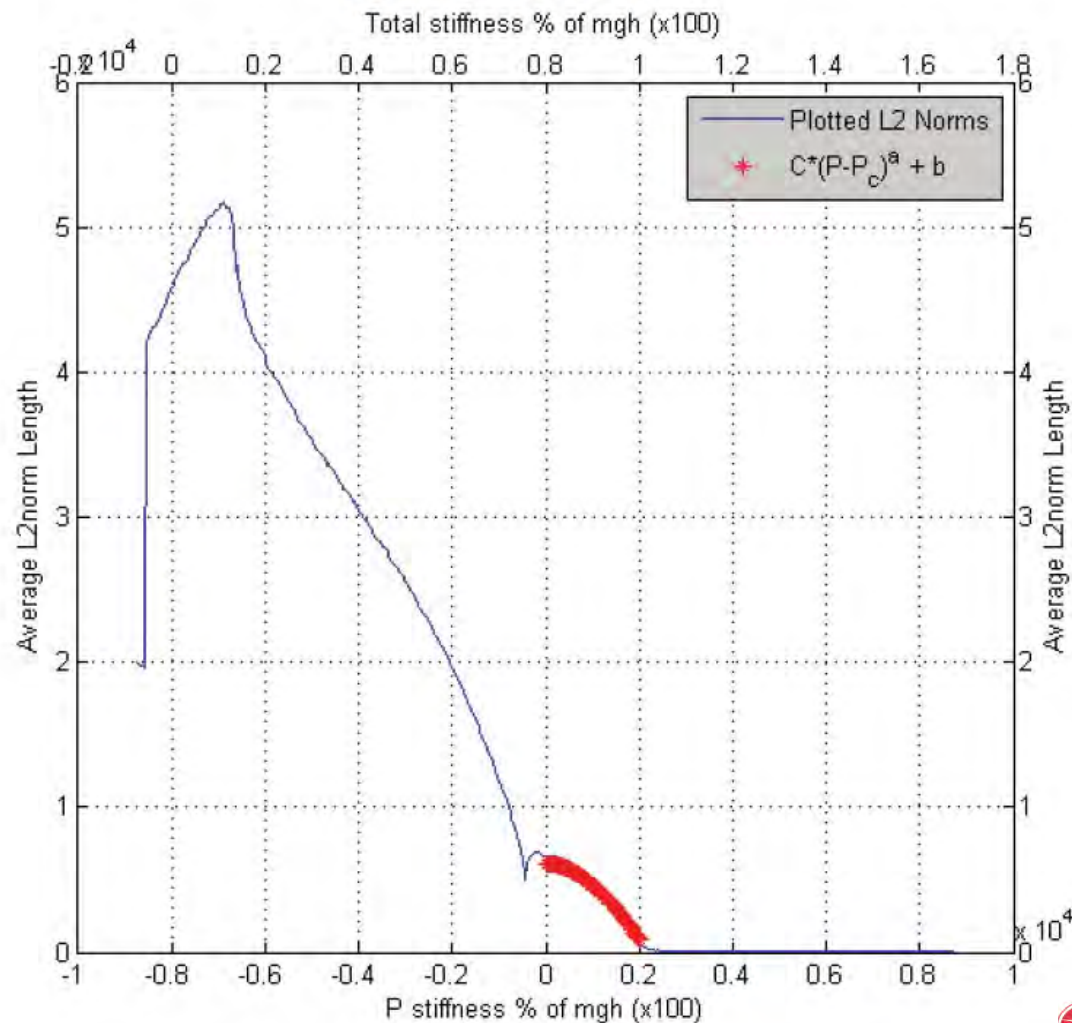
In this research

- Hypothesis 1: Aging can be modeled as change in parameters.
- Hypothesis 2: L2-Norm can be used as a balance metric.

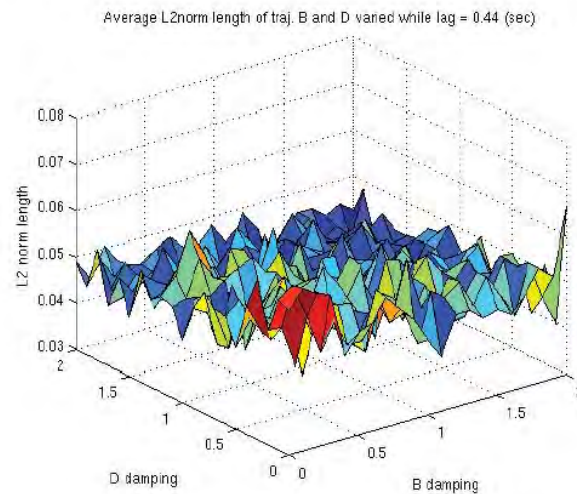
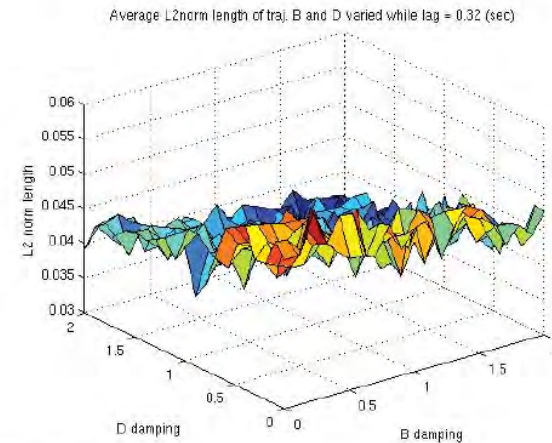
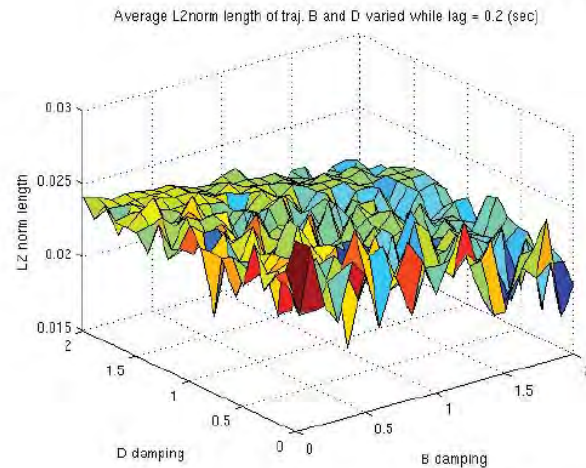
Linear Stability Analysis of 1 DOF



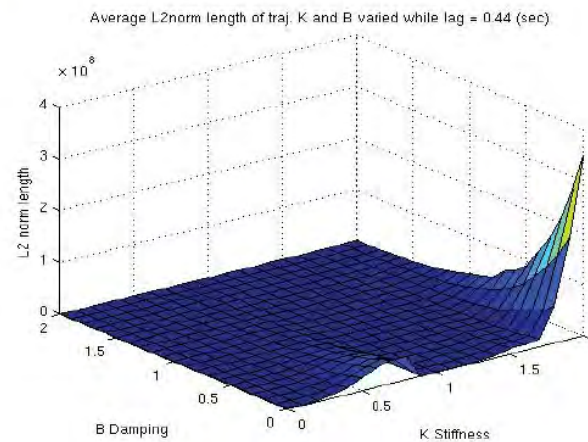
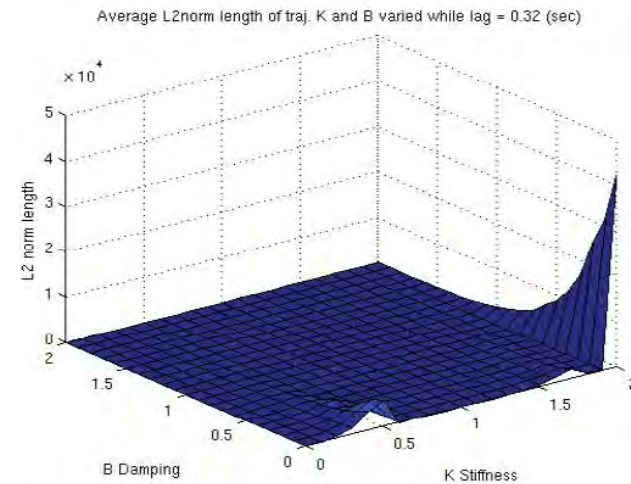
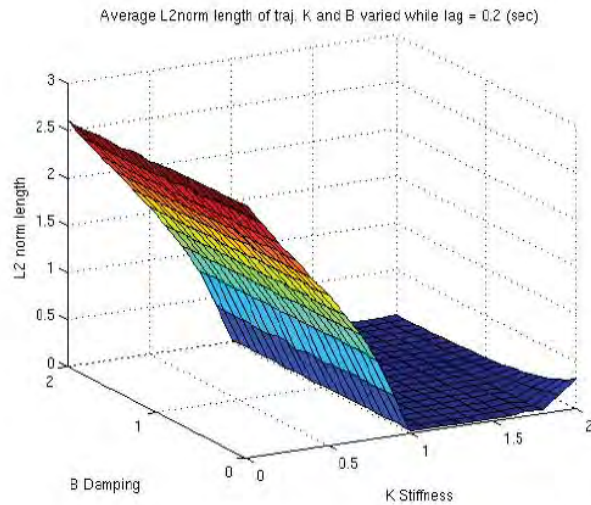
Parametric Study of One DOF Model



Parameter Combination Study of One DOF Model

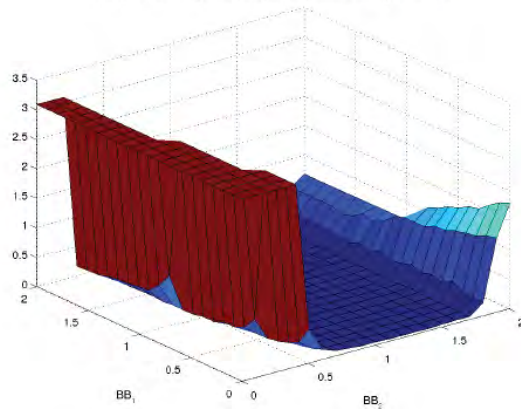


Parameter Combination Study of One DOF Model (cont'd)

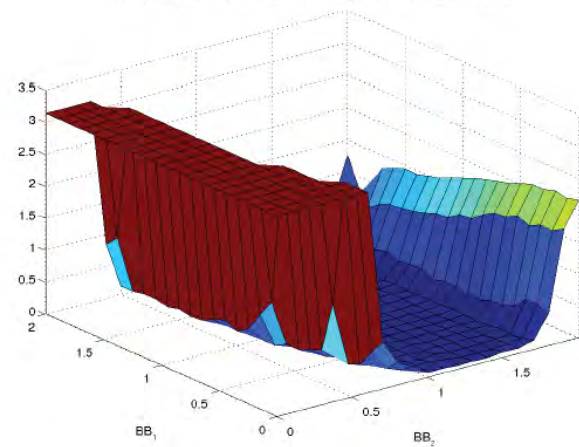


Parameter Combination Study of Two DOF Model

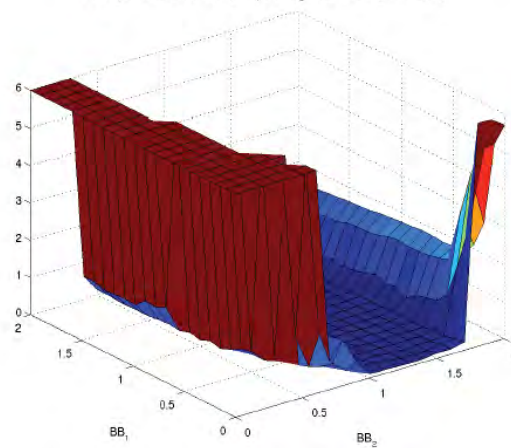
Average L2norm Length of traj. BB_1 and BB_2 varied while lag = 0.20 (sec)



Average L2norm Length of traj. BB_1 and BB_2 varied while lag = 0.32 (sec)

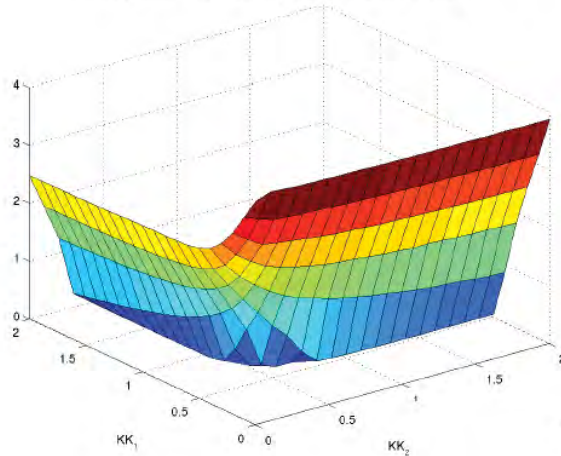


Average L2norm Length of traj. BB_1 and BB_2 varied while lag = 0.44 (sec)

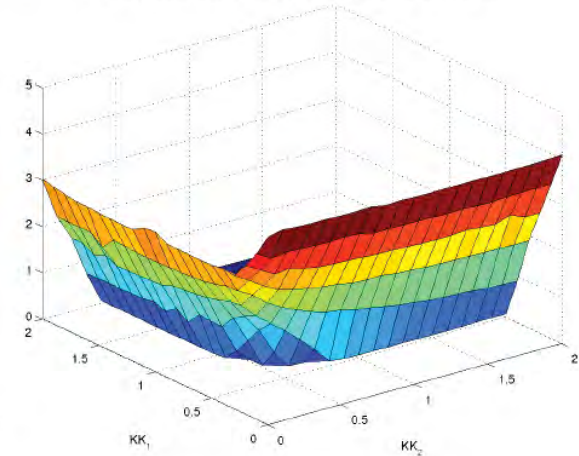


Parameter Combination Study of Two DOF Model (cont'd)

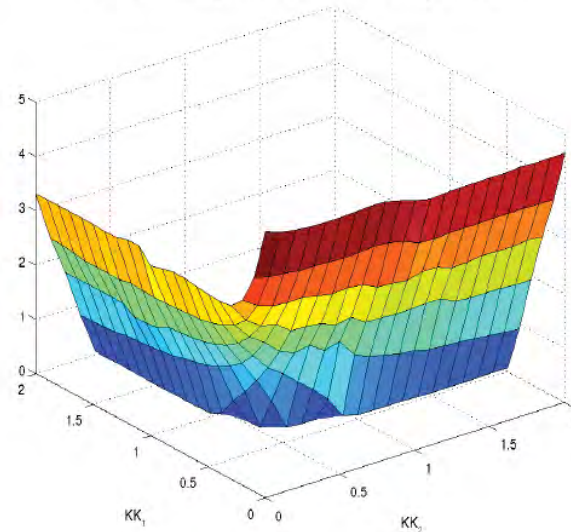
Average L2norm Length of traj. KK_1 and KK_2 varied while lag = 0.20 (sec)



Average L2norm Length of traj. KK_1 and KK_2 varied while lag = 0.32 (sec)



Average L2norm Length of traj. KK_1 and KK_2 varied while lag = 0.44 (sec)



Discussion

- L2 –Norm is useable metric for balance.
- Parametric studies show definite trends and sensitivities.
- Model choice dictates predictive capability as the strategy of balance can change with age.

Many more results in MS Thesis by Carson Willey (see Ohio Link)



The Nonlinear Dynamics of Quiet Standing in Humans

Willey, Carson Landis

Future Work

- Correlation with clinical/experimental data.
- Inclusion of normal forms into the parametric variations for balance.