

Nanoparticle inhalation alters systemic arteriolar vasoreactivity through sympathetic and cyclooxygenase-mediated pathways

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Abstract

The widespread increase in the production and use of nanomaterials has increased the potential for nanoparticle exposure; however, the biological effects of nanoparticle inhalation are poorly understood. Rats were exposed to nanosized titanium dioxide aerosols (10 µg lung burden); at 24 h post-exposure, the spinotrapezius muscle was prepared for intravital microscopy. Nanoparticle exposure did not alter perivascular nerve stimulation (PVNS)-induced arteriolar constriction under normal conditions; however, adrenergic receptor inhibition revealed a more robust effect. Nanoparticle inhalation reduced arteriolar dilation in response to active hyperaemia (AH). In both PVNS and AH experiments, nitric oxide synthase (NOS) inhibition affected only controls. Whereas cyclooxygenase (COX) inhibition only attenuated AH-induced arteriolar dilation in nanoparticle-exposed animals. This group displayed an enhanced U46619 constriction and attenuated iloprost-induced dilation. Collectively, these studies indicate that nanoparticle exposure reduces microvascular NO bioavailability and alters COX-mediated vasoreactivity. Furthermore, the enhanced adrenergic receptor sensitivity suggests an augmented sympathetic responsiveness.

Keywords: Microvascular, sympathetic nervous system, whole-body inhalation, nitric oxide, titanium dioxide

Introduction

Cardiovascular toxicity following inhalation of particulate matter (PM) is well established in the literature. General toxicity associated with PM exposure is enhanced as particle size decreases. As such, ultrafine particles and nanoparticles have been suggested to have an augmented toxicity

compared with their larger counterparts (Stone et al. 2007). Nanotechnology is a burgeoning industry that is incorporated into our daily lives. Nanoparticles are classified as particles with a diameter of <100 nm in one dimension (Aitken et al. 2006) and have diverse applications in medical imaging, targeted drug delivery, anti-cancer therapy, as well as properties that are useful in the manufacturing of goods such as surface coatings, UV protectorates, among others (Aitken et al. 2006). However, without first properly identifying their potential for biological effects, the ubiquitous inclusion of these materials in everyday products significantly raises the risk of personal and occupational exposure that may be intentional or accidental. Nanotechnology has tremendous potential to contribute positively to society; however, for this to fully occur, the health effects of these materials must first be defined (Maynard et al. 2006).

Nano-TiO₂ is used in products such as photocatalysts (Sun et al. 2004), antibacterial surface coatings (Shieh et al. 2006), as well as in cosmetics and sunscreens (Aitken et al. 2006). These particles induce relatively minor levels of inflammation following pulmonary deposition, but nevertheless the biological effect is dose dependent (Nurkiewicz et al. 2008). Generally, inhalation of nano-TiO₂ results in diffuse alveolitis with some increases in phagocytic cell recruitment and oedema (Nurkiewicz et al. 2008). However, the pulmonary effects are relatively minor compared with other occupationally relevant particles such as residual oil fly ash (Dreher et al. 1997).

Based on a vast epidemiological, clinical and animal toxicology literature, three major hypotheses have been promoted to explain the remote cardiovascular effects following inhalation of particles. These are (1) particle translocation into the systemic circulation and direct particle-tissue interactions (Oberdorster et al. 2004), (2) systemic

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inflammation leading to peripheral effects (Tamagawa et al. 2008) and (3) alterations in autonomic nervous system (ANS) activity to elicit peripheral effects (Stone & Godleski 1999). While all three mechanisms may be important, the vast majority of investigations have focused on systemic inflammation. Indeed, our laboratory has previously demonstrated that inflammation-mediated microvascular dysfunction follows particle exposure (Nurkiewicz et al. 2004, 2006). However, efforts to re-establish normal microvascular function through depletion of peripheral neutrophils or elimination of oxidant stress have only been partially successful (Nurkiewicz et al. 2008, 2011).

The critical role of the microcirculation in maintaining homeostasis, particularly in vital organs such as the brain and heart, cannot be overstated. The arteriolar network is the principal site of vascular resistance. Reactivity at this level of the microvasculature to a host of influences maintains optimal perfusion through the capillary network to ensure adequate gas, nutrient and waste exchange for proper tissue and organ function. Furthermore, many diseases, such as hypertension, are microvascular in origin (Vicaut 1999). Hence, not only is the microcirculation important in maintaining homeostasis, but it is also, unfortunately, the origin of many pathological processes. Tissue perfusion at the microvascular level is regulated through a complementary (and sometimes redundant) system of intrinsic and extrinsic pathways. Arteriolar tone is the net result of their combined influences, and subtle changes in this active generation of arteriolar tone have profound influence on tissue perfusion. As such, altered responses to these vasoactive influences (or stimuli) can disturb tissue perfusion and, therefore, tissue homeostasis. Hence, the complex interplay between these intrinsic and extrinsic factors that control tissue perfusion is of paramount importance in regard to the systemic microvascular effects that follow nanoparticle exposure.

Arteriolar blood flow in skeletal muscle is controlled through the interplay between central (i.e. neural), hormonal and local mechanisms of blood flow control to achieve optimal capillary perfusion based on local metabolic demand (Segal 2005). At rest, perfusion is largely limited by sympathetic nerve activity, but during activity, it is increased, due to production and accumulation of vasoactive metabolites. These metabolites override the influence of sympathetic activity in arterioles inducing active hyperaemia (AH), which is an increase in blood flow that accompanies an increase in metabolic activity (Kurjiaka & Segal 1995; Segal 2005). However, blood flow can still be limited by sympathetic nerve activity, since metabolic influences induce vasodilation but do not eliminate sympathetic nerve activity (Kurjiaka & Segal 1995). Therefore, enhanced sympathetic tone can limit the ultimate metabolic capacity of a given

tissue and therefore increase systemic blood pressure (Segal 2005).

Thus, the purpose of this study was to evaluate alternate pathways that may contribute to the microvascular dysfunction that follows nanoparticle inhalation and determine whether there is interaction between these pathways. Hence, our hypothesis is that the microvascular dysfunction associated with pulmonary nanoparticle exposure is not due entirely to endothelium-dependent mechanisms, but rather a dysfunction created by the combination of endothelium-dependent and endothelium-independent mechanisms.

Methods

Animals

Male Sprague Dawley rats (7–9 weeks old) were purchased from Hilltop Labs and housed in an Association for Assessment and Accreditation of Laboratory Animal Care International-approved animal facility at the National Institute for Occupational Safety and Health. Food and water were provided *ad libitum*. Additionally, male Sprague Dawley rats (7–9 weeks old) were purchased from Harlan Labs and housed in a PHS-approved animal facility at the West Virginia University Health Sciences Center. Because of animal housing restrictions, scheduling conflicts and facility resources, the control and nano-TiO₂ exposure groups contained a larger proportion of rats from either Hilltop Labs or Harlan Labs, respectively. As such, the animal vital statistics reflect a slight difference between the exposure groups (Table I). While these animals are of the same strain, these vendor-specific animals were delivered at slightly different ages, and because of vendor-specific growth curve differences, the age and weight statistics are different in Table I. However, our laboratory has previously shown that the microvascular reactivity is equivalent in male Sprague Dawley rats from these two vendors (Nurkiewicz et al. 2006). Furthermore, these groups, despite a slight difference in age, are both distinctly in the middle of a juvenile developmental stage (Linderman & Boegehold 1998). All animal procedures were performed on an approved protocol by the Institutional Animal Care and Use Committees at the National Institute for Occupational Safety and Health and West Virginia University.

Particles

The nano-TiO₂ powder was obtained from Degussa (Evonik, Aeroxide TiO₂, P25, primary particle size 21 nm, Parsippany, NJ). The powder was an approximate mixture of 80/20 of anatase/rutile (Nurkiewicz et al. 2008; Sager et al. 2008; Sager & Castranova 2009). The specific surface area of the particle was 48.08 m²/g as measured by the BET gas absorption

Table I. Animal characteristics.

Experimental group	Animal number	Age (days)	Weight (g)	MAP (mm Hg)	SBP (mm Hg)	DBP (mm Hg)	HR (BPM)
Control	39	58 ± 1	241 ± 1	100 ± 1	121 ± 1	89 ± 1	359 ± 1
Nano-TiO ₂	43	50 ± 1*	257 ± 1*	108 ± 1*	127 ± 1*	99 ± 1*	381 ± 1*

**p* < 0.05 vs. control by ANOVA, Data ± SE.

DBP, diastolic blood pressure; HR, heart rate; MAP, mean arterial pressure; SBP, systolic blood pressure.

technique (Sager et al. 2008) The nano-TiO₂ powder was carefully prepared for generation by drying (to avoid agglomerate formation due to high humidity), sieving (to remove the large agglomerates) and storage (to prevent agglomerate attraction through contact charges) as previously described (Nurkiewicz et al. 2008).

Whole-body inhalation exposure

National institute for occupational safety and health

Aerosols were generated by a fluidised bed as previously described (Nurkiewicz et al. 2008). Briefly, animals were exposed to a 138 nm count geometric mean diameter particle (D_p) aerosol with a final concentration of 6 mg/m³ of nano-TiO₂ for 4 h/day for 1 day. Real-time particle concentrations were monitored with a Data-RAM and confirmed gravimetrically with Teflon filters. This inhalation exposure concentration and duration has been shown previously to produce diffuse alveolitis with slight increases in phagocytic cell recruitment and oedema without producing overload (Nurkiewicz et al. 2008). Twenty-four h after nano-TiO₂ exposure, intravital microscopy was performed.

West virginia university

Nano-TiO₂ aerosols were generated with a vibrating fluidised bed, a Venturi vacuum pump and a cyclone separator (Figure 1) patent pending #61/455,355. The dry powder rested on a filter supported by a metal air distributor in the vibrating fluidised bed. The Venturi vacuum pump connected to the exit port of the fluidised bed has a high-velocity air jet blowing across a constriction in a pipe to create a suction that draws air and agglomerates of the particles into the Venturi vacuum pump. The large agglomerates were broken up by impaction and high-speed shear

flow in the Venturi vacuum pump. After the Venturi vacuum pump, the aerosols enter a cyclone separator with a cut-off diameter of 400 nm at input flow rate of 60 l/min. Most large agglomerates were removed from the aerosol flow before entering the exposure chamber. The 0.5 m³ exposure chamber (TSE, Bad Homburg, Germany) input air flow rate was 90 l/min with a pressure of -0.2 mbar. The animals were exposed 4 h/day for 1 day at a final concentration of 5.7 ± 0.25 mg/m³ (Figure 2). The real-time size distribution and relative mass concentration of the particles in the chamber were monitored between 7 and 10,000 nm by an Electrical Low Pressure Impactor (ELPI, Dekati, Tampere, Finland) and the count mean aerodynamic diameter (D_{ae}) was determined to be 160 nm (Figure 3A). Frequency distribution of particle size based on number/cm³ was derived from the ELPI data and overlaid with the actual particle number frequency distribution (Figure 3B). Real-time particle size distribution was also determined and between 14 and 670 nm (Figure 3C) by a Scanning Mobility Particle Sizer (SMPS, TSI, Shoreview, MN) and D_p was determined to be 160 nm. As above, frequency distribution of particle size based on number/cm³ was derived from the SMPS data and overlaid with the actual particle number frequency distribution (Figure 3D). These frequency distributions allow data above the 670 nm cut-off of the SMPS assumed based on a presumed normal distribution. The particle mass concentrations were confirmed gravimetrically with Teflon filters. A calculated total pulmonary deposition was estimated to be 30 μ g using both steady-state nanoparticle concentration and area under the curve. Our exposure calculation were made and rounded to be conservative. After twenty-four hours post-exposure, this concentration of nano-TiO₂ yields a total measured pulmonary deposition of 10 μ g (Nurkiewicz et al. 2008).

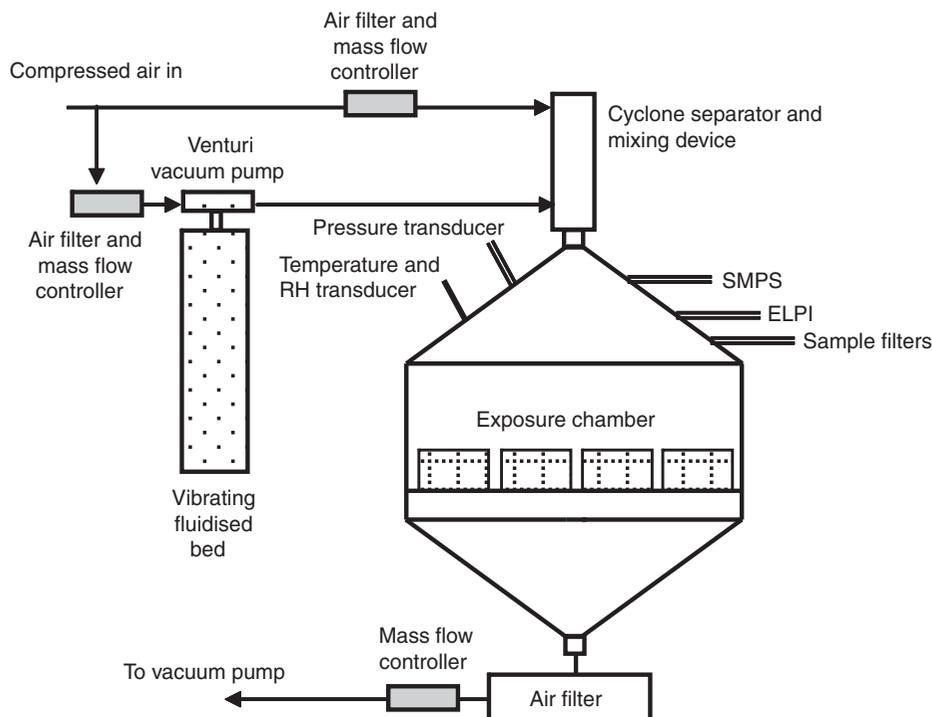


Figure 1. West Virginia University inhalation exposure facility schematic for the generation of nano-TiO₂ aerosols.

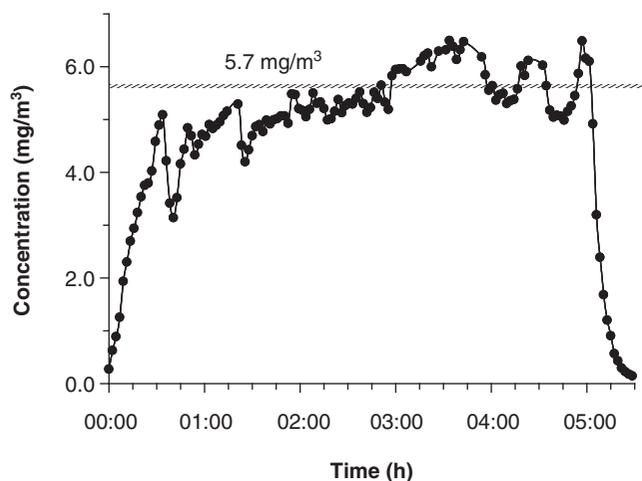


Figure 2. Real-time nano-TiO₂ concentrations over the exposure period. Dots represent 2-min averages with an average particle concentration of 5.7 mg/m³.

Particle sizes and concentrations used in the two exposure environments were slightly different; however, the particle composition and estimated dose were the same. As such, the results from these two exposures were similarly interpreted.

Intravital microscopy

Intravital microscopy was performed as previously described (Nurkiewicz et al. 2004). Rats were anaesthetised by an i.p. injection of sodium thiopental (100 mg/kg) and placed on a heating pad to maintain a rectal temperature of 37°C. The trachea was intubated to ensure a patent airway, and the right carotid artery was cannulated to measure arterial pressure. The right spinotrapezius muscle was exteriorised for microscopic observation, leaving feed vessels and innervation intact. The muscle was then gently secured over a clear pedestal at its *in situ* length and enclosed in a tissue bath and continuously superfused with an electrolyte solution (119 mM NaCl, 25 mM NaHCO₃, 6 mM KCl and 3.6 mM CaCl₂, pH 7.4, 290 mOsm), warmed to 35°C and equilibrated with 95% N₂, 5% CO₂. Superfusion flow rate was maintained at 4–6 ml/min to minimise equilibration with atmospheric oxygen (Boegehold & Bohlen 1988). The preparation was then transferred to the stage of an Olympus intravital microscope (Model BX51WI, Center Valley, PA) coupled to a CCD camera (Olympus Model DP71) and was observed under a 20X water immersion objective (final image magnification was 743X.). One to three arcade bridge arterioles were studied per animal preparation. These arterioles are the

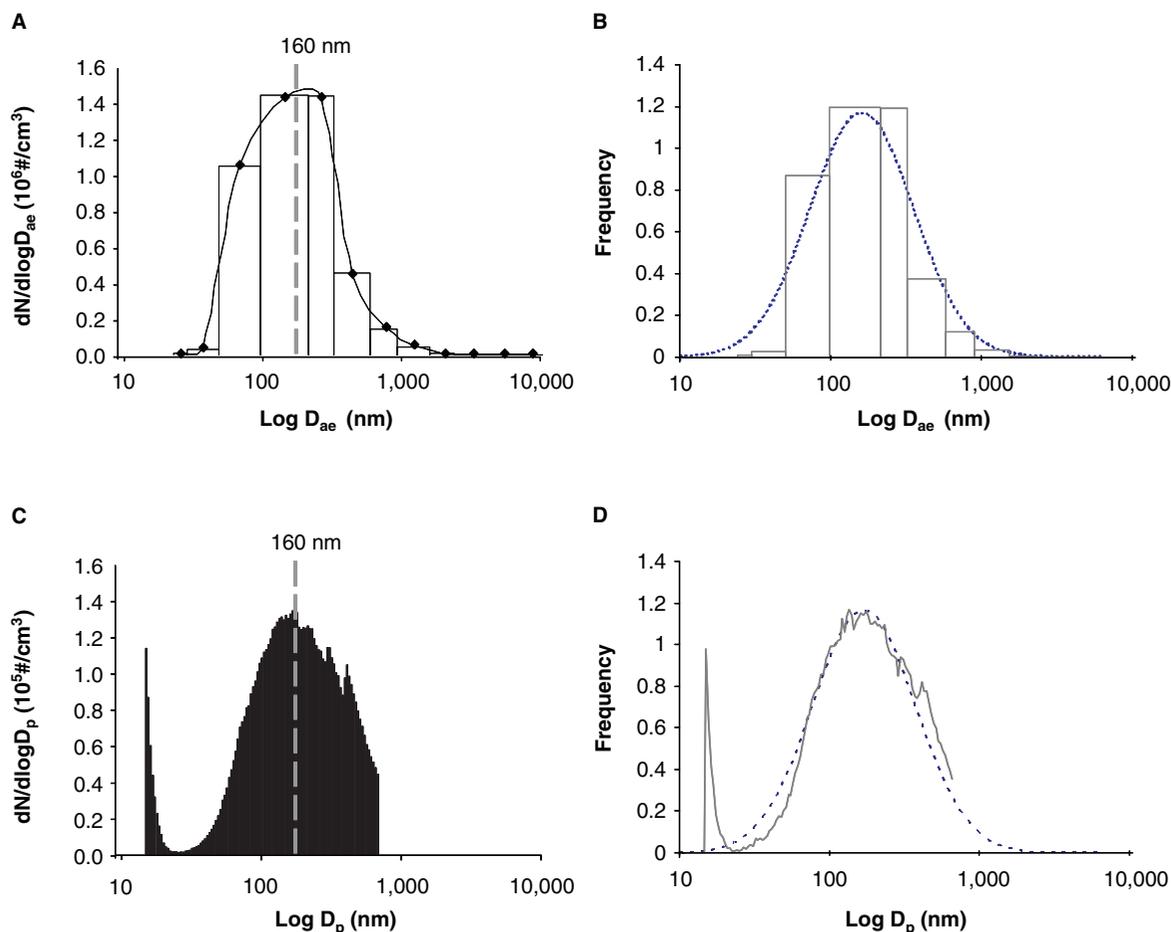


Figure 3. Nano-TiO₂ particle size distribution. (A) Representative ELPI size distribution of the nano-TiO₂ aerosol for the 13 impactor stages (between 7 and 10,000 nm). Average nano-TiO₂ aerosol count median aerodynamic diameter (D_{ae}) was 161 nm. (B) Gaussian distribution of particle size based on frequency. The dotted line is the model fit for a lognormal distribution function with a median (or geometric mean) of 160 nm and a geometric standard deviation of 2.2. The lighter grey line is the actual data from the ELPI. (C) Representative SMPS size distribution curve for the nano-TiO₂ aerosol over the 107 size cut-offs (between 14 and 670 nm). Average nano-TiO₂ aerosol count geometric mean diameter (D_p) was 159 nm. (D) The dotted line is the model fit for a lognormal distribution function with a median (or geometric mean) of 160 nm and a geometric standard deviation of 2.2. The solid lighter grey line is the actual data from the SMPS.

site of the majority of vascular resistance in the spinotrapezius muscle and hence of major importance in regulation of blood flow in the muscle (Boegehold 1991). The arcade bridge arteriole originates from the thoracodorsal and 11th intercostal arteries at the proximal and distal ends, respectively, of the muscle forming a loop that contributes the entire blood supply for the arcading vascular network (Schmid-Schonbein et al. 1991). Real-time images were displayed on a high-resolution computer monitor. Greater than three images were digitally captured via DP Controller (Olympus, Center Valley, PA) during a baseline period and immediately following each experimental period. Arteriolar diameters from each digital image were determined by Microsuite analysis software (Olympus, Center Valley, PA) calibrated with a stage micrometer. Arteriolar diameters were averaged per experimental end point to reduce sampling variability.

Superfusate chemicals

Compounds were introduced via a syringe pump at 1/10 of the flow rate (i.e. 0.4–0.6 ml/min). *N*^G-monomethyl-L-arginine (L-NMMA, Calbiochem, Gibbstown, NJ) was used at a final tissue bath concentration of 100 μM to inhibit NOS activity (Nase & Boegehold 1997a; Linderman & Boegehold 1998). Meclofenamate (MEC, Sigma-Aldrich, St. Louis, MO) was used at a final concentration of 30 μM to inhibit COX activity (Nase & Boegehold 1997b; Linderman & Boegehold 1998). The final tissue bath concentration of phentolamine (Sigma-Aldrich, St. Louis, MO), an α-adrenergic receptor blocker (Kurjiaka & Segal 1995; Nase & Boegehold 1997b; Linderman & Boegehold 1998), and tetrodotoxin (Sigma-Aldrich, St. Louis, MO) (Kurjiaka & Segal 1995; Linderman & Boegehold 1998), a fast sodium channel blocker that inhibits all nerve function, was 1 μM. Superfusate concentrations of these inhibitors have been previously shown to be effective in the spinotrapezius muscle preparation (Kurjiaka & Segal 1995; Lash 1995; Nase & Boegehold 1997b; Linderman & Boegehold 1998; Marvar et al. 2005). U46619 and iloprost (Cayman Chemical, Ann Arbor MI) were superfused at a final concentration of 1–100 nM or 2.8–28 nM, respectively (Didion et al. 1997; Xiang et al. 2006). Adenosine (ADO, Sigma-Aldrich, St Louis, MO) was superfused at the end of the experiments (100 μM) to determine passive arteriolar diameters.

Statistics

Arteriolar diameter (*D*, in micrometres) was recorded during a control or perivascular nerve stimulation (PVNS) period and immediately following AH or during superfusion with pharmacological agents. Resting vascular tone was calculated for each vessel as follows: $\text{tone} = [(D_{\text{pass}} - D_c)/D_{\text{pass}}] \cdot 100$, where D_{pass} is passive diameter under ADO and D_c is the diameter measured during the control period. A tone of 100% represents complete vessel closure, whereas 0% represents the passive state. Arteriolar responses were normalised as follows: percent change from control = $[(D_{\text{ss}}/D_c) - 1] \cdot 100$, where D_{ss} is the steady-state diameter following AH and PVNS or during tissue superfusion. All data are reported as mean ± SE. Statistical analyses were performed with

commercially available software (Sigmastat; Chicago, IL). Two-way repeated measures ANOVA was used to determine the effects of group, treatment and group-treatment interactions on measured variables. For all ANOVA procedures, the Student–Newman–Keuls post-hoc analysis was used to identify pair-wise differences among specific groups. Significance was assessed at the 95% confidence level ($p < 0.05$) for all tests.

Experimental protocols

Protocol 1

PVNS was performed on arcade bridge arterioles to determine responsiveness to sympathetic nerve stimulation. To accomplish this, a bevelled micropipette was filled with 0.9% saline and attached to a Grass current programmer. The tip of the micropipette was brought to gently rest in the adventitia of the arteriole to be studied. The perivascular nerves were stimulated for 20–60 sec to develop stable constriction at a randomly assigned frequency of 2, 4, 8 or 16 Hz. This stimulation protocol has been previously demonstrated to produce stable vasoconstriction without inducing escape during the stimulation period (Kurjiaka & Segal 1995). The observation site was distal to the stimulation site by 2–5 mm in the direction of flow to ensure that the effects of stimulation were neural in origin and not from depolarisation of the vascular smooth muscle cells, as previously described (Kurjiaka & Segal 1995; Linderman & Boegehold 1998). Microvascular reactivity was assessed first under normal superfusate conditions, then in the presence of L-NMMA, MEC, phentolamine or tetrodotoxin. Arterioles were allowed to recover a minimum of 2 min between stimulations to return to baseline diameters following each randomly assigned frequency.

Protocol 2

AH was induced in a separate set of rats through the stimulation of muscular contraction to determine the impact of nanoparticle exposure on metabolically induced vasodilation. To induce muscular contraction, electrodes were attached to the rostral and caudal ends of the spinotrapezius muscle to stimulate the muscle at 2, 4, 8 and 12 Hz at 0.2 msec in duration at 3–6 V for 1 min as previously described (Lash & Bohlen 1987). Voltage was determined empirically for each animal preparation to produce the maximum contraction in the muscle (Lash & Bohlen 1987). Variables that influenced voltage were primarily animal weight and muscle length. Most of our experiments were conducted at 5V. The frequencies used in the protocol have been shown to be below the threshold for direct excitation of vascular smooth muscle or autonomic neurons as well as being non-tetanic (Lash & Bohlen 1987). Frequencies 2–8 Hz are physiologically relevant with the suprphysiological stimulation of 12 Hz performed to maximally produce vasoactive metabolites (Lash & Bohlen 1987). Superfusate inhibitors (L-NMMA, MEC and phentolamine) were added following normal superfusate responses to determine mechanistic changes in microvascular reactivity. Tetrodotoxin was not evaluated since at 1 μM the compound at this concentration inhibits normal skeletal muscle contraction. Arterioles were

allowed to recover a minimum of 2 min between stimulations to return to baseline diameter following each randomly assigned frequency.

Protocol 3

A separate set of rats were prepared for intravital microscopy. Baseline images were collected for each arcade bridge arteriole studied, and then the muscle was superfused with either U46619 or iloprost for 10 min per dose. Following each randomly assigned dose, images of each arcade bridge arteriole were taken and the microvascular network was allowed to recover and return to baseline for at least 10 min following each dose. Following all protocols and at the end of the experiment, the muscle was superfused with ADO for 10 min to determine D_{pass} .

Results

Microvessel characteristics

Arteriolar diameter and tone under normal superfusate conditions were not different between control and nano-TiO₂-exposed animals (Table II). The various superfusate treatments did not alter arteriolar diameter or tone except for phentolamine treatment in the nano-TiO₂-exposed group. Superfusion with this α -adrenergic antagonist significantly increased arteriolar diameter and reduced tone only in the nanoparticle-exposed group (Table II).

Nanoparticle exposure alters response to α -adrenergic stimulation

To determine whether nanoparticle exposure augments the influence of the sympathetic nervous system on arteriolar constriction, perivascular nerves associated with arcade bridge arterioles were stimulated in control and nano-TiO₂-exposed animals (Figure 4). Under the normal superfusate, nanoparticle exposure did not appear to alter perivascular nerve-mediated constriction (max $-36\% \pm 3$ control, $-32\% \pm 2$ nano-TiO₂, 16 Hz (Figure 4A)). However, inhibition of NOS via L-NMMA superfusion enhanced arteriolar constriction in control animals but did not alter this constriction in nano-TiO₂-exposed animals ($-57\% \pm 5$ control, $-39\% \pm 7$ nano-TiO₂, 16 Hz (Figure 4B)). Arteriolar constriction was overtly blunted with α -adrenergic blockade in both the nano-TiO₂-exposed animals and control animals at 8 and 16 Hz compared with the normal superfusate treatment (max response $-24\% \pm 6$ control, $-9\% \pm 2$ nano-TiO₂ (Figure 4C)). Nano-TiO₂

exposure increased sensitivity to α -adrenergic blockade compared with control arterioles at 8 and 16 Hz (Figure 4C). Ablation of all nerve activity with tetrodotoxin rendered arteriolar reactivity to PVNS unresponsive in both the groups (Figure 4D). All frequency modulations for both control and nano-TiO₂-exposed animals superfused with tetrodotoxin were significantly different from the respective normal superfusate equivalents (Figure 4D), suggesting pharmacological ablation of nerve function completely disrupts changes in PVNS-induced arteriolar constriction. Arteriolar dilation induced by PVNS in the presence of tetrodotoxin, which has been demonstrated previously (Linderman & Boegehold 1998), was not different between control and nano-TiO₂-exposed animals. Inhibition of COX, via MEC superfusion, did not alter responses in control or nano-TiO₂-exposed animals (data not shown).

Nanoparticle exposure blunts active hyperaemia

Spinotrapezius muscle arteriolar responses to increased metabolic demand were frequency dependent (Figure 5). Exposure to nano-TiO₂ particles significantly reduced vasodilation at 12 Hz compared with control animals (max $183\% \pm 13$ control, $144\% \pm 15$ nano-TiO₂ (Figure 5A)). The addition of an NOS inhibitor significantly blunted vasodilation in the control animals but not in nano-TiO₂-exposed animals at 8 and 12 Hz (max $61\% \pm 12$ control, $152\% \pm 17$ nano-TiO₂ (Figure 5B)), suggesting a reduction in NO bioavailability in the nano-TiO₂-exposed animals. Inhibition of COX with MEC significantly reduced arteriolar dilation in nano-TiO₂-exposed animals at 8 and 12 Hz while not altering dilation in control arterioles (max $179\% \pm 27$ control, $71\% \pm 17$ nano-TiO₂ (Figure 5C)), suggesting a COX-mediated compensation for the reduced NO bioavailability in the nano-TiO₂-exposed animals.

Nanoparticle inhalation alters sensitivity to COX products

Because the balance of vasoactive factors following AH appeared to be more dependent on a COX-mediated pathway after nano-TiO₂ exposure, the relative sensitivity of these arterioles to COX product mimetics was determined. Superfusion of the thromboxane A₂ (TxA₂) mimetic, U46619, led to a dose-dependent vasoconstrictive effect (Figure 6A). The overall vasoconstrictive effect of U46619 was greater in the nano-TiO₂-exposed animals at 1 nM compared with control, indicating a greater sensitivity to TxA₂ (Figure 6A). Conversely, the prostacyclin analogue iloprost led to a

Table II. Characteristics of all arterioles studied.

Superfusate	Control			Nano-TiO ₂		
	<i>n</i>	Diameter (μm)	% Tone	<i>n</i>	Diameter (μm)	% Tone
Normal	59	34 \pm 1	66 \pm 1	71	34 \pm 1	68 \pm 1
L-NMMA	17	32 \pm 2	65 \pm 3	16	32 \pm 2	69 \pm 2
Meclofenamate	15	35 \pm 3	68 \pm 3	17	36 \pm 2	66 \pm 2
Phentolamine	18	30 \pm 2	70 \pm 2	23	41* \pm 4	63* \pm 3
Tetrodotoxin	4	29 \pm 2	65 \pm 3	9	31 \pm 2	65 \pm 4
Passive diameter	59	102 \pm 2		71	107 \pm 3	

* $p < 0.05$ vs. control arterioles; Data are means \pm SE; *n* = number of vessels per group.

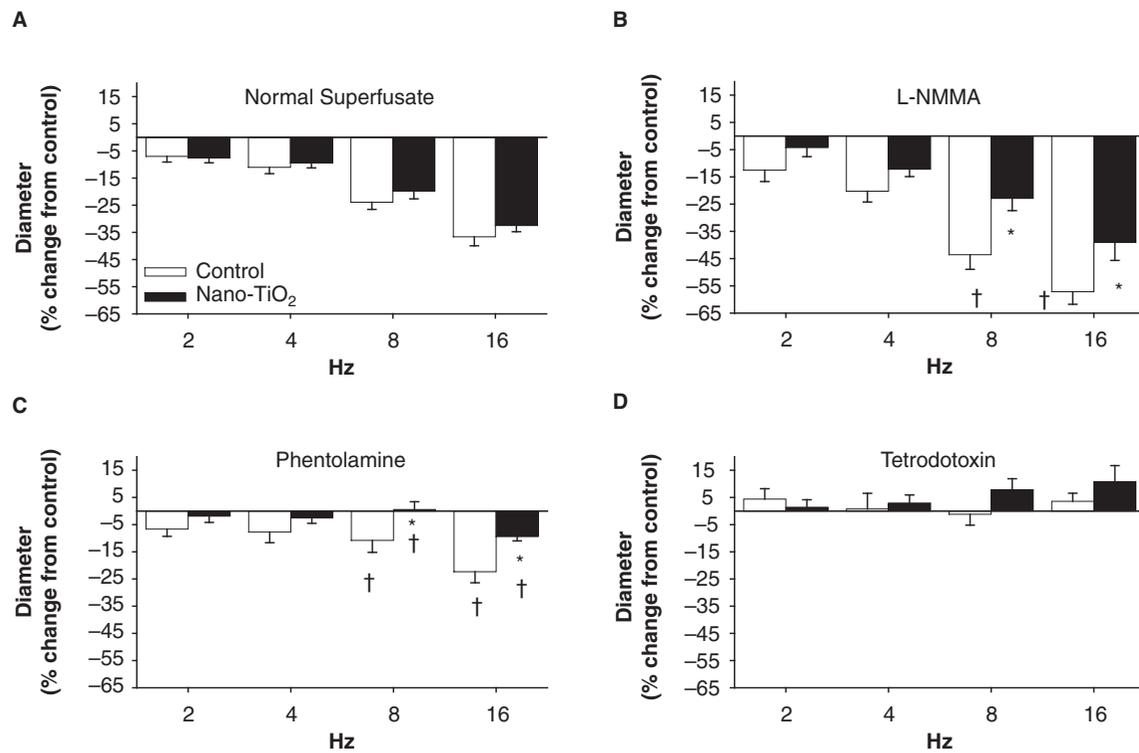


Figure 4. Nanoparticle inhalation alters arteriolar responsiveness to sympathetic stimulation following L-NMMA and phentolamine treatment. PVNS was performed as described in the Methods. (A) Nano-TiO₂ exposure did not alter responsiveness to sympathetic arteriolar constriction during normal PSS superfusion ($n = 23$ control, 27 nano-TiO₂-exposed arterioles). (B) Treatment with L-NMMA increased arteriolar constriction in control animals but not nano-TiO₂-exposed animals ($n = 10$ control, 12 nano-TiO₂-exposed arterioles). (C) Nano-TiO₂ exposure increased sensitivity to α -adrenergic blockade during sympathetic arteriolar constriction ($n = 10$ control, 11 nano-TiO₂-exposed arterioles). (D) Tetrodotoxin significantly ablated arteriolar constriction in all groups ($n = 4$ control, 9 nano-TiO₂-exposed arterioles). Values are means \pm SE. * $p < 0.05$ vs. control at same stimulation frequency, † $p < 0.05$ vs. normal superfusate at the same frequency.

dose-dependent vasodilatory effect (Figure 6B). There was a decrease in sensitivity to iloprost superfusion at 2.8 nM in the nano-TiO₂-exposed rats compared with control (Figure 6B). These data suggest that, in addition to a possible COX-product compensation for the lack of NO bioavailability, nanoparticle exposure also alters sensitivity to COX products.

Nanoparticle exposure induces persistent sympathetically mediated arteriolar dysfunction

Phentolamine superfusion led to a significant vasodilatory effect in the nano-TiO₂-exposed arterioles (Table II). However, AH-induced vasodilation at 12 Hz continued to be impaired even in the presence of α -adrenergic blockade following nano-TiO₂ exposure (Figure 7). These data suggest that even during α -adrenergic receptor inhibition or in the absence of sympathetic influence, nanoparticle exposure stimulates vasoactive influences that favour arteriolar constriction, and this effect cannot be overcome by local metabolic influences.

Discussion

Alterations in vascular reactivity following particle inhalation have been consistently demonstrated in the literature (Nurkiewicz et al. 2004; Mills et al. 2005; Rundell et al. 2007; Shah et al. 2008; LeBlanc et al. 2010). However, it remains unclear through what mechanism(s) these effects occur. The

nanoparticle used in this study had minimal inherent pulmonary toxicity, as evidenced by no change in inflammatory proteins measured in bronchoalveolar lavage fluid and the relatively minor alveolar inflammation-induced following inhalation at total retained deposition of 10 μ g (Nurkiewicz et al. 2008). Given the ubiquitous inclusion of TiO₂ in everyday products, this particle is relevant to both occupational (Madl & Pinkerton 2009) and personal exposures (Newman et al. 2009). Nano-TiO₂ exposure (1) augmented arteriolar α -adrenergic receptor sensitivity, (2) decreased the influence of NO on sympathetic nerve-mediated arteriolar constriction, (3) impaired arteriolar responsiveness to metabolic stimuli and (4) altered either the balance of or arteriolar sensitivity to COX products.

Similar to other vascular beds, sympathetic efferents project into the spinotrapezius microvasculature and terminate at approximately the third-order arcade arterioles (Todd 1980; Marshall 1982). We stimulated these neurons via PVNS to produce arteriolar constriction in a graduated manner that was frequency dependent (Figure 4). These arterioles exhibited sensitivity to α -adrenergic receptor antagonism following nanoparticle inhalation (Table II). This vasodilatory effect during α -adrenergic blockade suggests that an altered tonic sympathetic activity follows nanoparticle inhalation. It has been shown that at neurovascular junctions, neuropeptide Y, norepinephrine and perhaps ATP serve critical functions (Huidobro-Toro & Donoso 2004) and are important in sympathetic vasoconstriction (Coney & Marshall 2007).

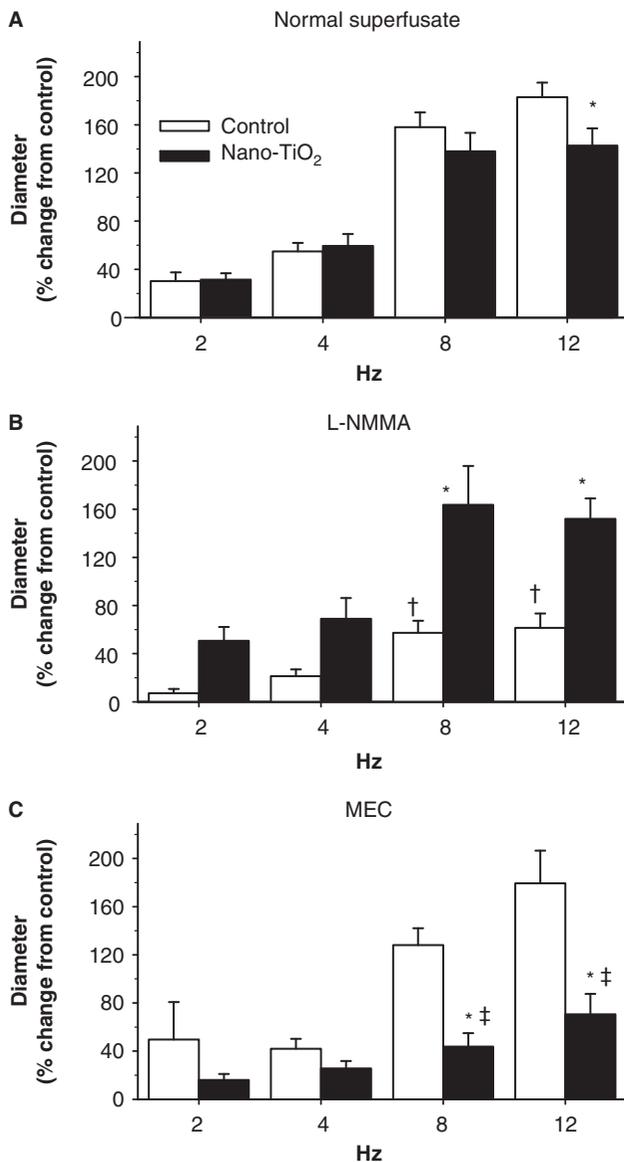


Figure 5. Nanoparticle inhalation attenuates functional arteriolar dilation during active hyperaemia. (A) Nano-TiO₂ exposure reduces arteriolar vasodilation to metabolic stimuli ($n = 23$ control, 31 nano-TiO₂-exposed arterioles). (B) Inhibition of NO production with *N*^G-monomethyl-L-arginine (L-NMMA) attenuates arteriolar dilation in control animals but not nano-TiO₂ exposed ($n =$ eight control, nine nano-TiO₂-exposed arterioles). (C) Conversely, inhibition of cyclooxygenase impairs arteriolar dilation in nano-TiO₂-exposed animals compared with control ($n = 9$ control, 15 nano-TiO₂-exposed arterioles). MEC, meclofenamate. Values are means \pm SE. * $p < 0.05$ vs. control, † $p < 0.05$ vs. control normal superfusate at the same frequency, ‡ $p < 0.05$ vs. nano-TiO₂-exposed normal superfusate at the same frequency.

Additionally, the enhanced sensitivity in nanoparticle exposed animals to α -adrenergic receptor blockade during PVNS (Figure 4C) may suggest a predominance of norepinephrine-mediated constriction.

Several studies have demonstrated a reduction in NO bioavailability in humans (Mills et al. 2005; Tornqvist et al. 2007; Shah et al. 2008) and in animal toxicological studies (Nurkiewicz et al. 2006; Proctor et al. 2006; Knuckles et al. 2008). Basal arteriolar tone was not altered following superfusion with L-NMMA in control or nanoparticle-exposed animals (Table II), which is not surprising given

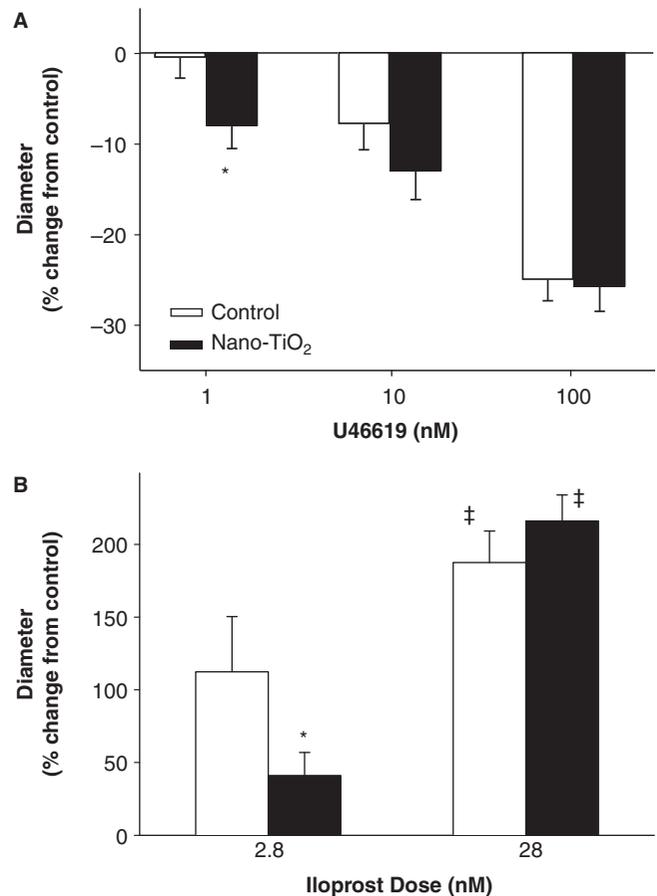


Figure 6. Pulmonary nanoparticle exposure alters arteriolar responsiveness to thromboxane A₂ (TxA₂) and prostacyclin mimetics. (A) Superfusion of the spinotrapezius muscle with U46619, a TxA₂ mimetic, significantly enhanced arteriolar constriction following nano-TiO₂ exposure compared with control animals at 1 nM ($n = 16$ control, 13 nano-TiO₂-exposed arterioles). (B) Iloprost superfusion led to a dose-dependent arteriolar dilation that was significantly blunted at 2.8 nM following nano-TiO₂ exposure (2.8 nM $n = 9$ control and $n = 13$ nano-TiO₂-exposed; 28 nM $n = 11$ control and $n = 16$ nano-TiO₂-exposed arterioles). Values are means \pm SE. * $p < 0.05$ vs. control exposure, ‡ $p < 0.05$ vs. 2.8 nM iloprost.

the multitude of extrinsic and intrinsic signals that regulate basal tone (Segal 2005). PVNS stimulation in the presence of the NOS inhibitor L-NMMA enhanced arteriolar constriction in control animals while not altering the responses in nanoparticle-exposed animals (Figure 4B). Similarly, inhibition of NOS activity blunted the hyperaemia-induced arteriolar dilation in control animals while not affecting arterioles from nanoparticle-exposed animals (Figure 5B). These data are consistent with previous reports that bioavailable NO reduces arteriolar constriction during PVNS (Linderman & Boegehold 1998) and is an important mediator of hyperaemia-induced vasodilation (Dua et al. 2009).

As discussed above, loss of NO bioavailability has been explored extensively in human and animal models either through endothelium-dependent or endothelium-independent mechanisms (Mills et al. 2005; Campen et al. 2005; Rundell et al. 2007; Knuckles et al. 2008; Shah et al. 2008; Cherng et al. 2009; Nurkiewicz et al. 2009). Furthermore, previous work by our laboratory and others has shown a consistent attenuation in both humans and animals of NO

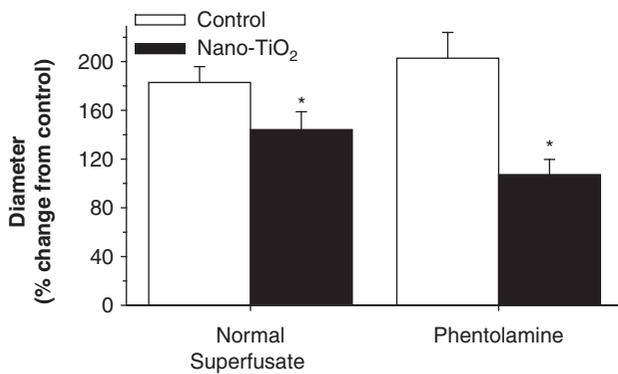


Figure 7. Nanoparticle inhalation exposure resulted in persistent blunting of arteriolar dilation without the influence of sympathetic nerves. α -Adrenergic blockade failed to alter the blunting of arteriolar dilation following active hyperaemia at 12 Hz in nano-TiO₂-exposed animals. Values are means \pm SE. * $p < 0.05$ vs. control exposure.

bioavailability following inhalation of particles that is likely reactive oxygen species related (Nurkiewicz et al. 2004; Mills et al. 2005; Nurkiewicz et al. 2006; Knuckles et al. 2008; Nurkiewicz et al. 2009; Cherng et al. 2011). Other mechanisms of vasodilation have not been as vigorously explored. However, obviously vascular function, however blunted, still exists. In humans, Mills et al. (2005) showed that relative vasoreactivity in arteries was altered to a range of mechanistically distinct compounds. Specifically, Mills and colleagues determined deficits in vasodilation following bradykinin, acetylcholine and sodium nitroprusside. These data highlight both a deficit in production of NO as well as utilisation of NO. Hence, the overall consensus of their work and others is that fine particles, nanoparticles or air pollutants limit vasodilation through reductions in NO bioavailability.

While several lines of evidence have demonstrated reductions in NO following particle exposure, none has shown a link between sympathetic influence and vascular function. Within the literature, limited data exist for altered sympathetic influence in the vasculature following particle exposure. Our laboratory was the first to report that inhibition of fast Na⁺ channels with tetrodotoxin partially restores endothelium-dependent arteriolar dilation in nano-TiO₂-exposed rats (Nurkiewicz et al. 2011). Within the broader literature, alterations in autonomic nervous system function (i.e. parasympathetic and sympathetic) have been largely confined to measures of heart rate variability (HRV). While these measures are essential in humans, their translation in rodent models is less clear, given the indirect nature of the measurement and the lack of testable mechanistic outcomes (Rowan, III et al. 2007).

While autonomic nervous system data with HRV measures can be difficult to interpret in animal studies, several epidemiological and clinical studies have clearly shown an increase in blood pressure following PM exposure (Brook et al. 2009; Liu et al. 2009). Furthermore, the increase in arterial blood pressure in both human and animal models appears to be diastolic in origin (Zanobetti et al. 2004; Bartoli et al. 2009; Brook et al. 2009). In a dog model, Bartoli et al. (2009) found that the transient increases in

blood pressure could be mitigated with the systemic addition of an α -adrenergic receptor blocker, prazosin, during PM exposure. Furthermore, the PM-exposed dogs had an altered baroreceptor reflex response compared with control. PM exposure also led to a prolongation of the R-R interval relative to increase in systolic blood pressure following transient infusion of phenylephrine. These data suggest that the origin of the increased blood pressure following particle inhalation is likely sympathetic. Furthermore, the increase in diastolic pressure indicates an increase in arteriolar resistance (Stouffer 2008). In our study, while baseline arteriolar diameters and tone were not altered under the normal superfusate condition between exposure groups, α -adrenergic blockade resulted in a significant dilation in the nanoparticle-exposed group (Table II). This suggests an increase in tonic sympathetic influence in our study that is consistent with results found by Bartoli et al. (2009). Furthermore, we hypothesise that based on the reported increases in diastolic blood pressure and the changes in tonic sympathetic influence, blood pressure would be altered in our animals following nanoparticle exposure. Our mean arterial pressure (MAP), systolic blood pressure (SBP), diastolic blood pressure (DBP) and heart rate (HR) measurements were different between control and nanoparticle exposed animals (Table I). However, it is not clear whether the effect was the result of the rats in the nanoparticle-exposed group having a larger mass and hence a slightly greater blood pressure and heart rate or an effect of nanoparticle exposure. The intravital microscopy technique employed in this study requires the use of anaesthesia, which makes it difficult to confidently extrapolate any differences in blood pressure and heart rate between groups. Future studies will incorporate arterial blood pressure measurements in telemetered conscious animals to determine whether nanoparticle inhalation exposure increases blood pressure.

In this study, we found that AH-induced vasodilation was significantly attenuated after nanoparticle inhalation. This suggests an alteration in the sensitivity, production or uptake of vasoactive metabolites, which may be partially due to a reduction in NO bioavailability. Further study revealed that the compensatory mechanism for this apparent loss in NO bioavailability is probably COX-mediated (Figure 5C). Furthermore, α -adrenergic blockade, while resulting in a vasodilatory effect at baseline (Table II), failed to normalise vasodilation to AH (Figure 7). While we expected α -adrenergic blockade to normalise AH-induced arteriolar dilation in the nanoparticle-exposed animals, an alternative explanation for the lack of normalisation would be that the effects of adrenergic stimulation continue to impair vasodilation even in the absence of new adrenergic signalling. Previous work by Faber & Meininger (1990) demonstrated that pre-exposure to adrenergic agonists predisposed tissues to hyperconstriction and led to a greater resistance to vasodilation even in the absence of changes in arteriolar tone (Faber & Meininger 1990). In the context of the present study, nanoparticle inhalation appears to enhance sympathetic influence, which is through an adrenergic pathway (Table II, Figure 4C). Hence, these data support a

predisposition towards vasoconstriction via an adrenergic mechanism, since α -adrenergic receptor antagonism failed to normalise metabolically induced vasodilation (Figure 7). Additionally, peroxyntirite, which is increased following nano-TiO₂ exposure (Nurkiewicz et al. 2008), has been shown to increase RhoA/Rho kinase activity (El-Remessy et al. 2010), which promotes calcium sensitivity in resistance arterioles (Bolz et al. 2003). The enhanced calcium sensitivity may play a role in the persistent attenuation of vasodilation observed following phentolamine treatment and AH-mediated vasodilation in nanoparticle-exposed animals (Figure 7). Furthermore, this is consistent with an augmented responsiveness to the calcium ionophore, A23187, following exposure to nanoparticles (Nurkiewicz et al. 2008; LeBlanc et al. 2009; Nurkiewicz et al. 2009).

TxA₂ is a potent vasoconstrictor and one of several metabolites of arachidonic acid that has been shown to play a significant role in platelet aggregation, bronchoconstriction and vasoconstriction (Dogne et al. 2004), as well as microvascular dysfunction (Goodwill et al. 2008a, 2008b). Increased sensitivity to TxA₂ can occur through increased receptor density (Dogne et al. 2004) as well as decreases in the formation of antagonistic arachidonic acid metabolites (Goodwill et al. 2008b). Some hallmarks of increased TxA₂ sensitivity have been shown in context to PM and nanoparticle exposures (e.g. enhanced vasoconstriction (Brook et al. 2002; Rundell et al. 2007), and platelet aggregation (Nemmar et al. 2008)). There appears to be an enhanced sensitivity to TxA₂ and a reduction in sensitivity to prostacyclin possibly leading to an overall pro-constrictive effect for COX mimetics following nanoparticle exposure (Figure 6). Hillslope analysis suggests a right-shifted EC₅₀ curve following exposure to nanoparticles (data not shown), but the biological relevance of this effect is unclear at this time. Moreover, the vasoreactivity data to COX mimetics should be interpreted with caution because a full dose range should be developed in future studies. Collectively, these data suggest an altered production of COX metabolites (Figure 5C) as well as altered prostanoid receptor activity, distribution and/or signalling mechanisms (Figure 6). Future studies should also determine the role of nanoparticle inhalation in altering COX product formation, prostanoid receptor distribution and alterations in COX isoform expression.

The reduction in NO bioavailability highlighted in this work, and previously demonstrated in this vascular bed following nanoparticle exposure (Nurkiewicz et al. 2009), appears to be compensated for through a shift to a COX-mediated mechanism. Previous work by LeBlanc et al. (2010) demonstrated in isolated coronary arterioles that nanoparticle inhalation exposure led to a slight vasoconstriction to arachidonic acid (the metabolic precursor to prostacyclin and TxA₂), whereas control arterioles exhibited vasodilation. Nanoparticle exposure did not alter vasoconstriction to U46619. Furthermore, coronary arteriolar endothelium-dependent vasodilation with acetylcholine following nanoparticle inhalation exposure was attenuated compared with control animals (LeBlanc et al. 2009, 2010). However, the

addition of L-NMMA or indomethacin (a preferential COX-1 inhibitor) did not alter vasodilation in the nanoparticle-exposed animals (LeBlanc et al. 2010). While not a complete investigation, these data in isolated coronary arterioles suggest that inhaled nanoparticles alter arteriolar vasoreactivity correspondingly across different vascular beds. Furthermore, flow-mediated dilation was nearly normal in coronary arterioles isolated from nanoparticle-exposed rat compared with control (LeBlanc et al. 2009). These data suggest that while impairments in NO-mediated vasodilation are present, compensatory mechanisms (e.g. COX products), or a shift in their contributions, at least partially preserve the functional vasoreactivity following nanoparticle exposure.

The dose relationship of these exposures in humans was highlighted in Nurkiewicz et al. (2009). Briefly, the occupational limit for fine TiO₂ is 5 mg/m³. Measured levels of nano-TiO₂ in a production plant are as high as 1.4 µg/m³. Thus, an equivalent pulmonary burden in human to 10 µg in the rat would be achieved in roughly 5 years (Nurkiewicz et al. 2009).

This study demonstrates that nanoparticle inhalation negatively impacts arteriolar tone and reactivity via mechanisms that are not exclusively endothelium-dependent. These data also highlight a reduction in responsiveness to metabolic stimuli as well as an altered tonic sympathetic influence. Furthermore, the normal vasodilatory NO signal is blunted following nanoparticle exposure, which is likely compensated for through a COX-mediated pathway. This study also highlights the need for a greater understanding of the complex changes in vascular physiology that result from particle exposure. While the effects of particle exposure on vascular reactivity have been largely described through a reduction in NO bioavailability, generation of vascular resistance is a mechanistically complex interplay of a variety of influences and will require continued comprehensive investigations of all avenues of vasoregulation. Future studies should focus on measuring sympathetic nerve activity following exposure to nanoparticles, as well as using therapeutic interventions to prevent nanoparticle-induced microvascular dysfunction.

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Declaration of interest

The author reports no conflicts of interest. The author alone is responsible for the content and writing of the paper.

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